

# X-ray Tomography

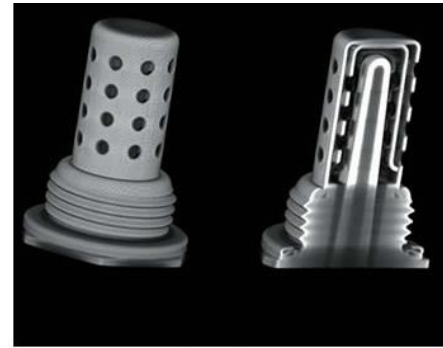
Navid Asadi

Physical Inspection and Attacks on ElectronicS (PHIKS)

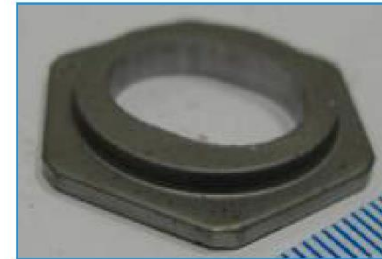
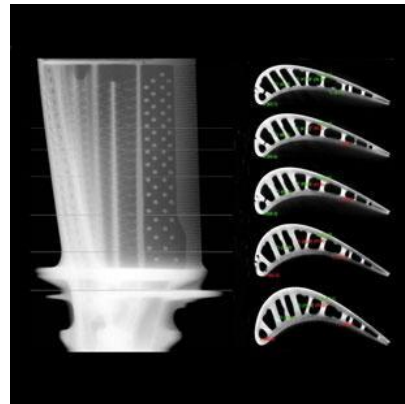
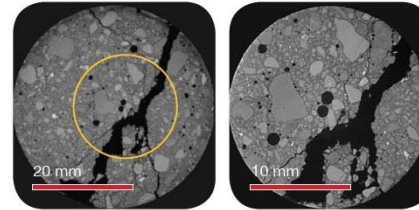
# X-ray Scanning

## Non Destructive Testing

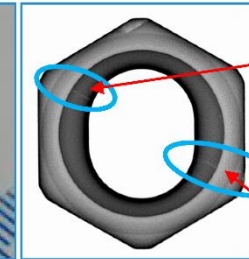
- Medical applications
- Automobile industry
- Aerospace inspection
- Oil and gas
- Batteries
- Electronics



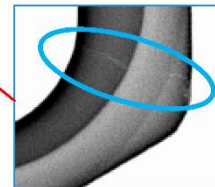
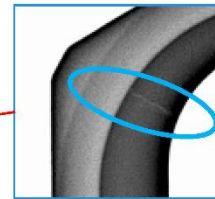
Oxygen Sensor



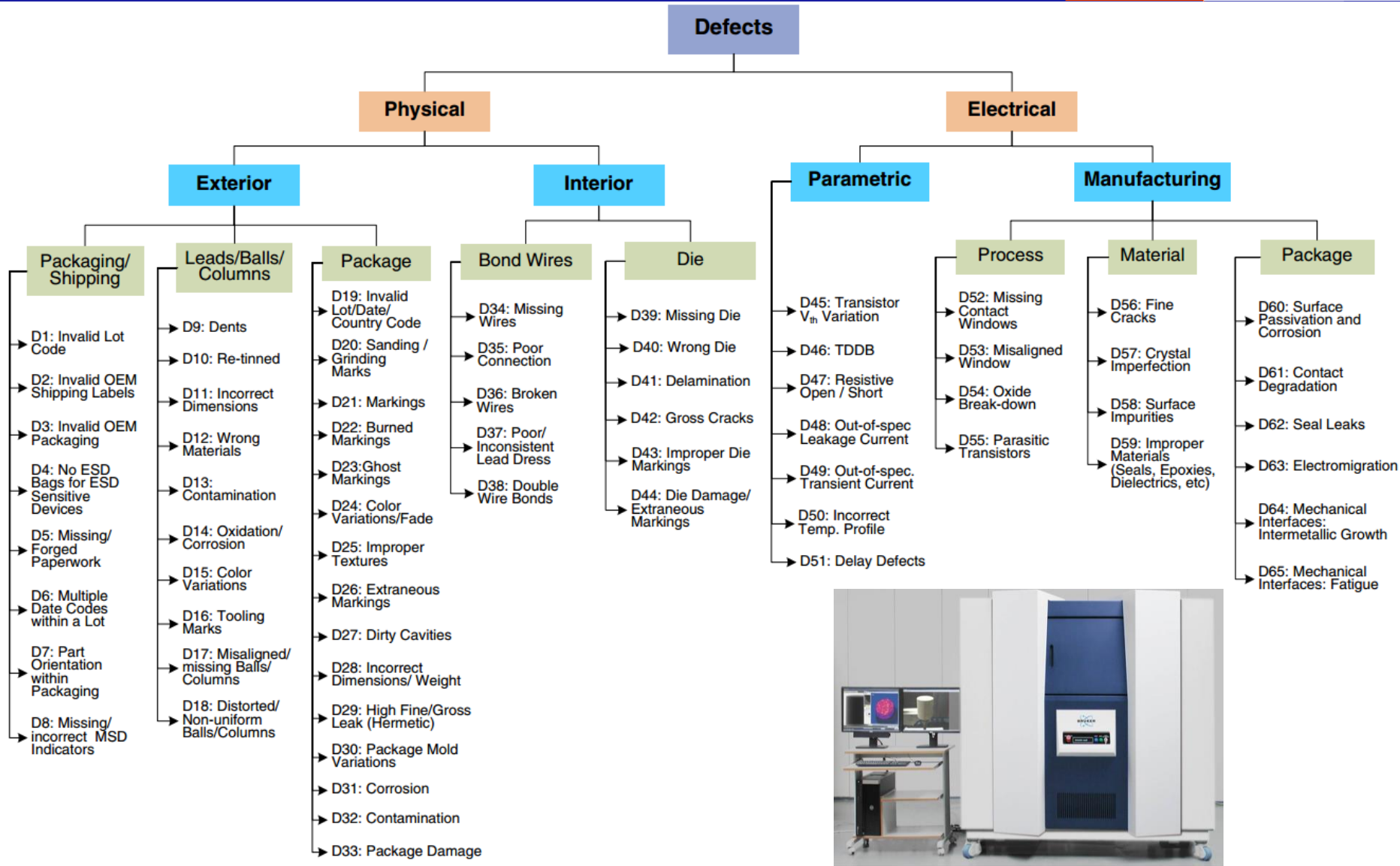
(a)



(b)

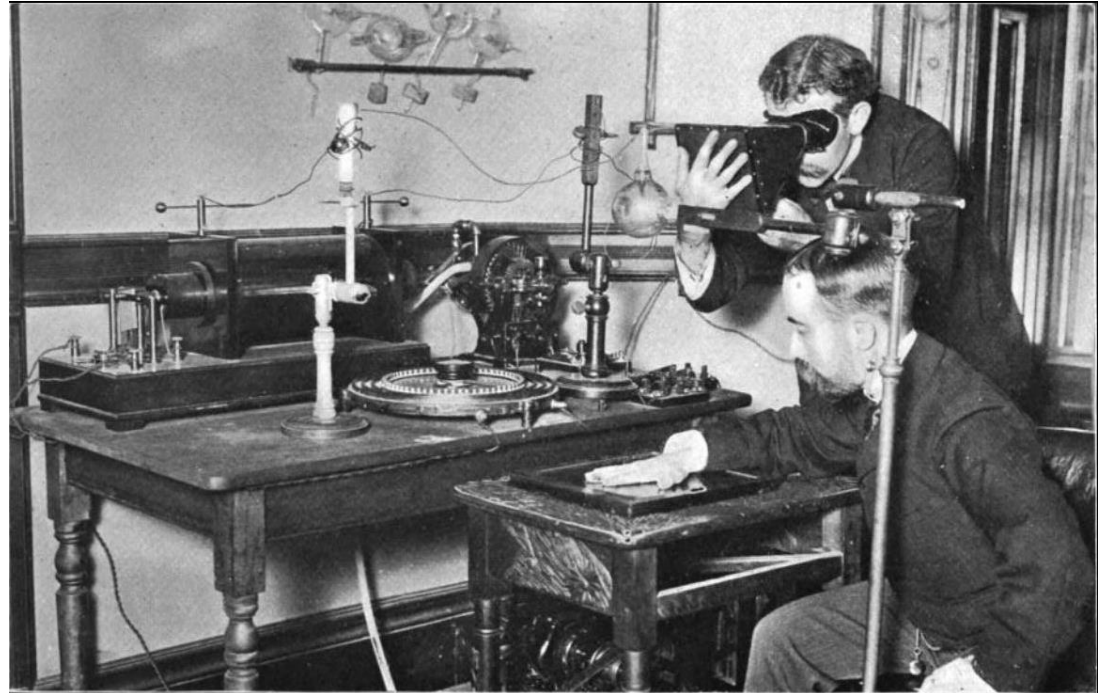


# Taxonomy of Defects



# X-rays Discovery

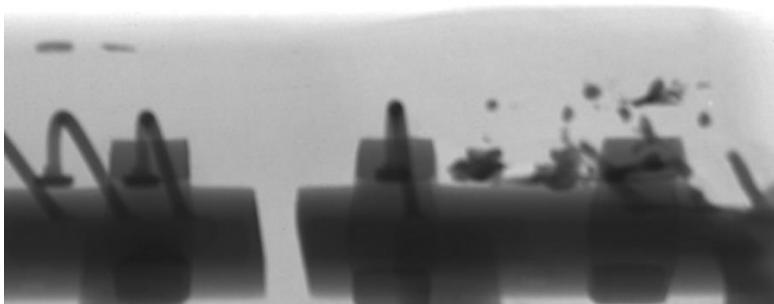
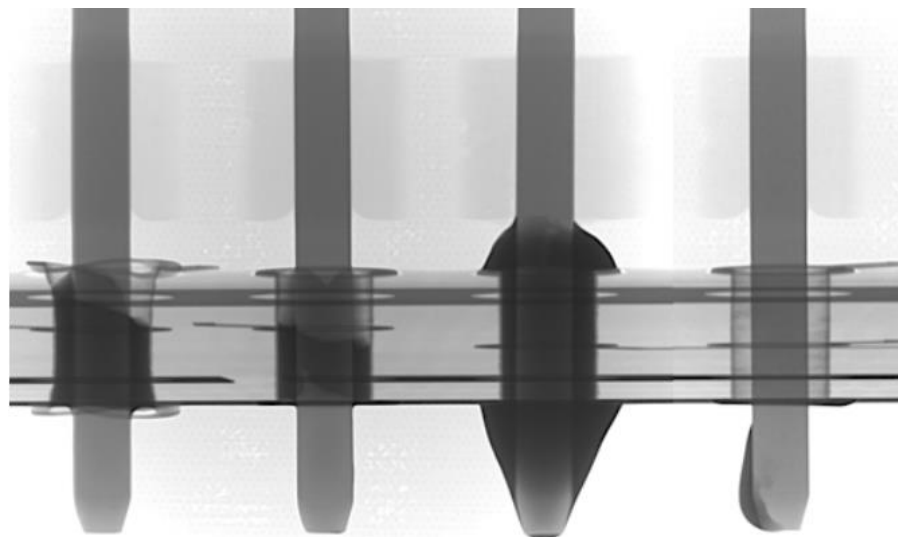
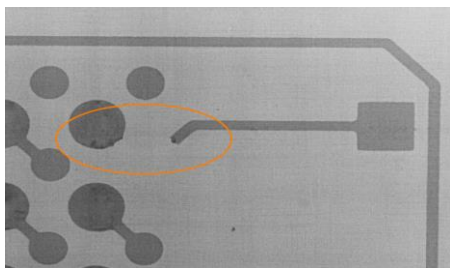
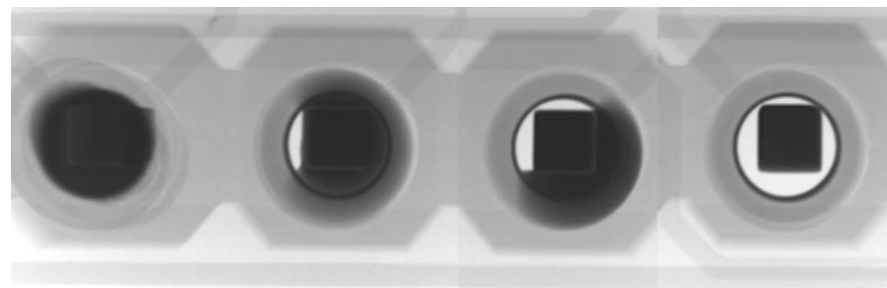
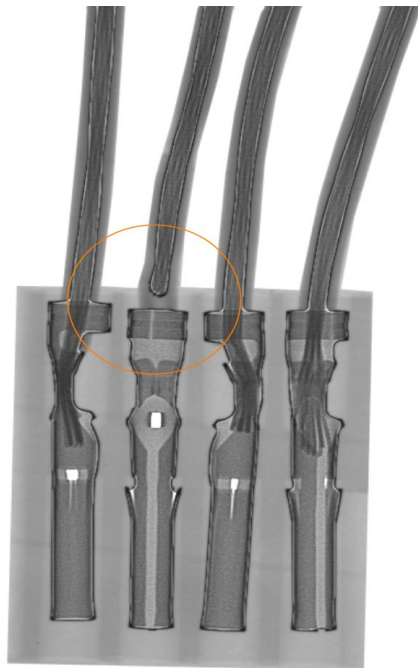
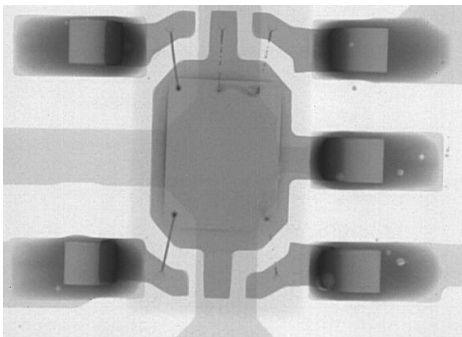
First X-ray image by German physicist, Wilhelm Röntgen, 1895



- First X-ray image application for medical purposes
- No precautions against radiation exposure were taken



# 2D X-ray Inspection



# What is X-ray Computed Tomography?

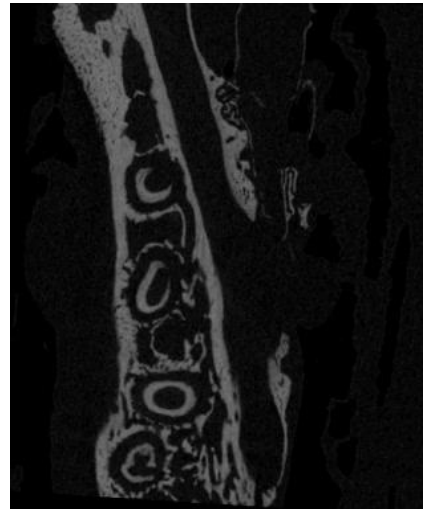
## 1. “Scan”

A set of x-ray “projection” images are taken over a rotation of the imaging axis of 180 or 360 degrees



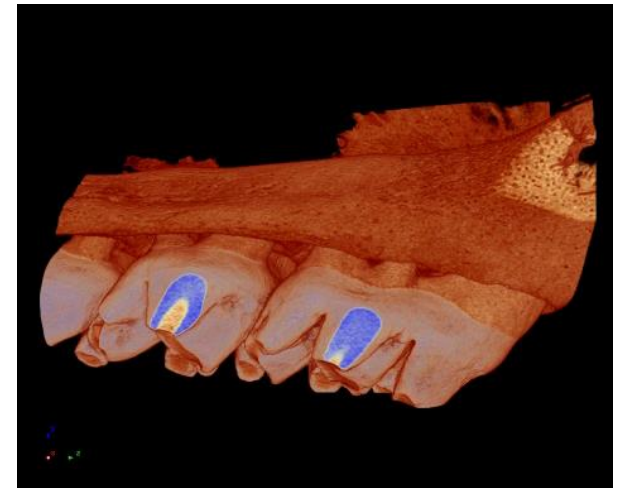
## 2. “Reconstruction”

The “projection” images are processed by the filtered Feldkamp cone-beam method to create the stack of cross-section slices



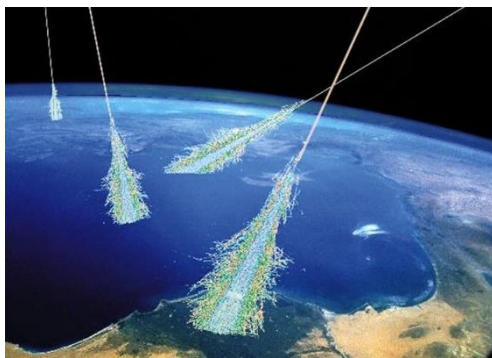
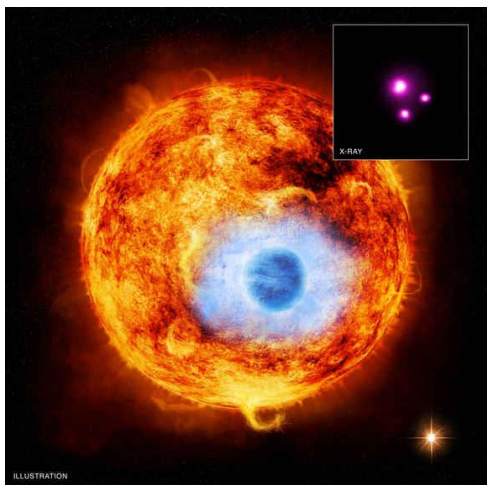
## 3. “Analysis and visualisation”

The reconstructed cross-section slices are processed into 3d models for morphometric measurements and virtual visual inspection

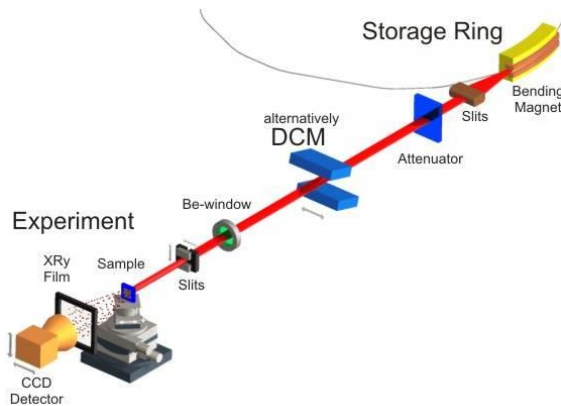
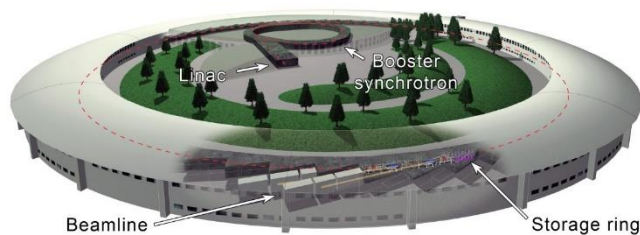


# How are X-rays Produced?

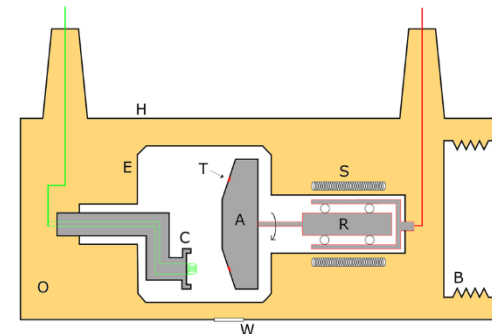
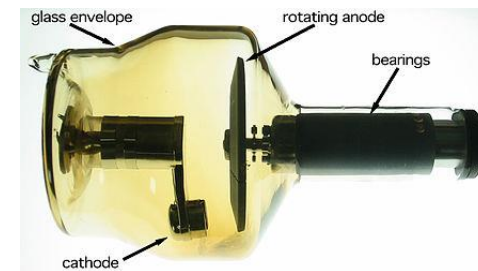
## Cosmic Events



## Synchrotron

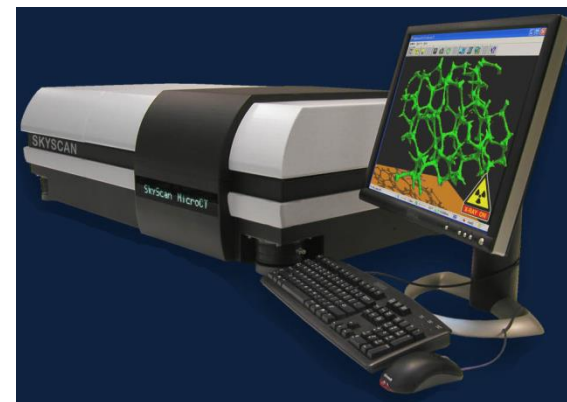
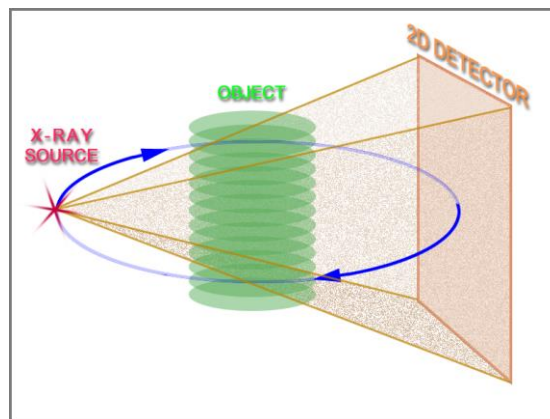


## Laboratory

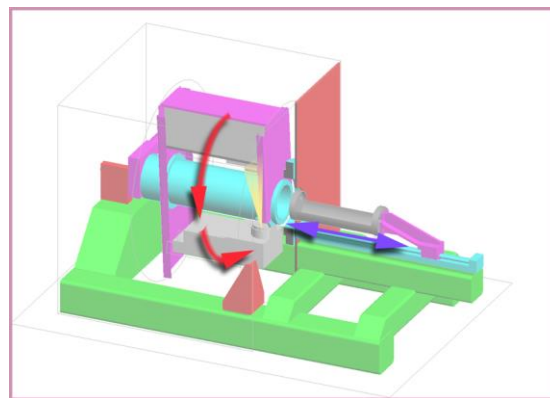


# *in vivo* and *ex vivo* Methods

In the “*ex vivo*” scanner type, the sample rotates on a stage around a vertical axis, allowing angular projection images over 360 degrees



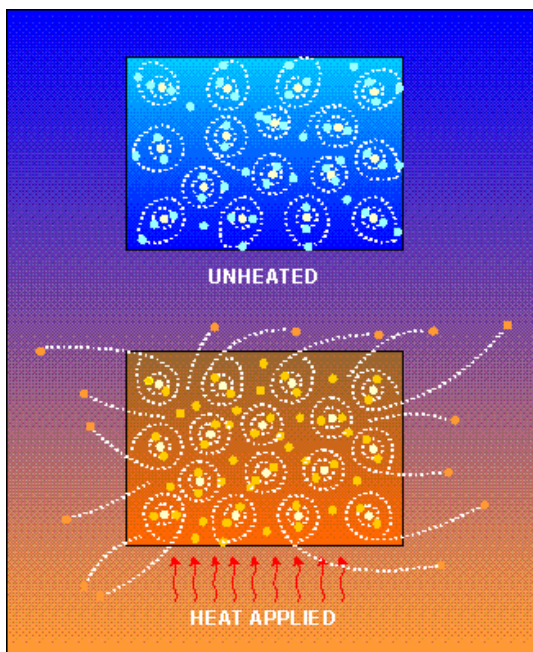
In the “*in vivo*” scanner type, the sample – e.g. a live mouse or rat – lies still on a horizontal bed, while x-ray source and camera rotate around the sample bed, over 360 degrees





# How are X-rays Produced?

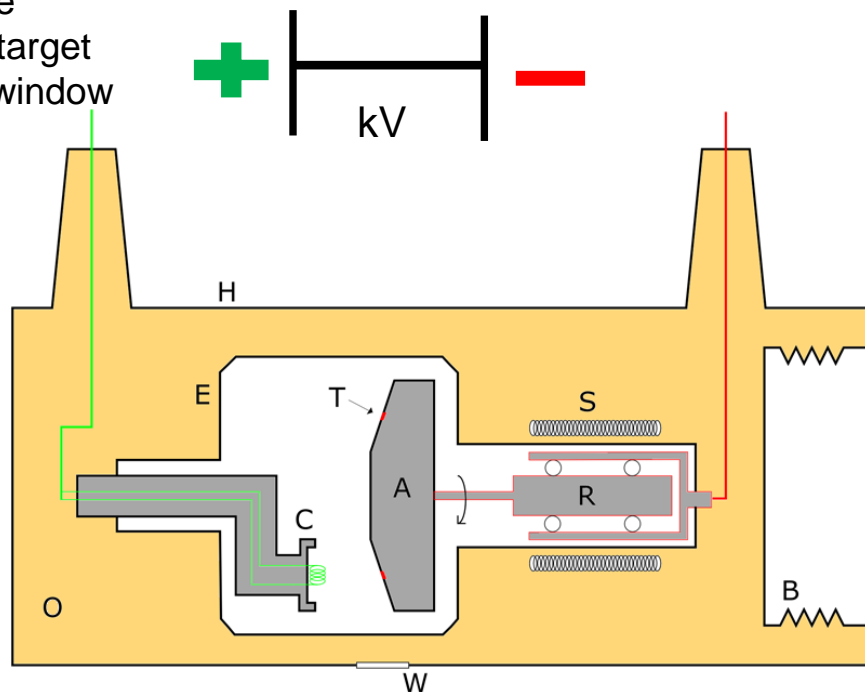
## X-ray Emission



### Thermionic Emission:

Filament is heated until the electrons can escape

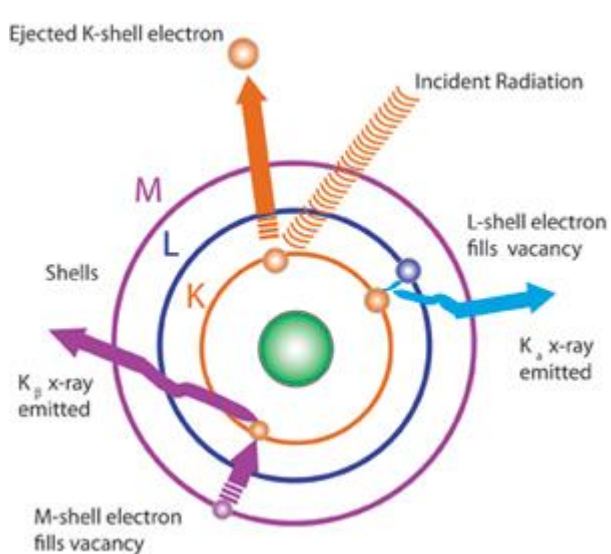
- Simplified rotating anode tube schematic
- A: Anode
- C: cathode
- T: Anode target
- W: X-ray window



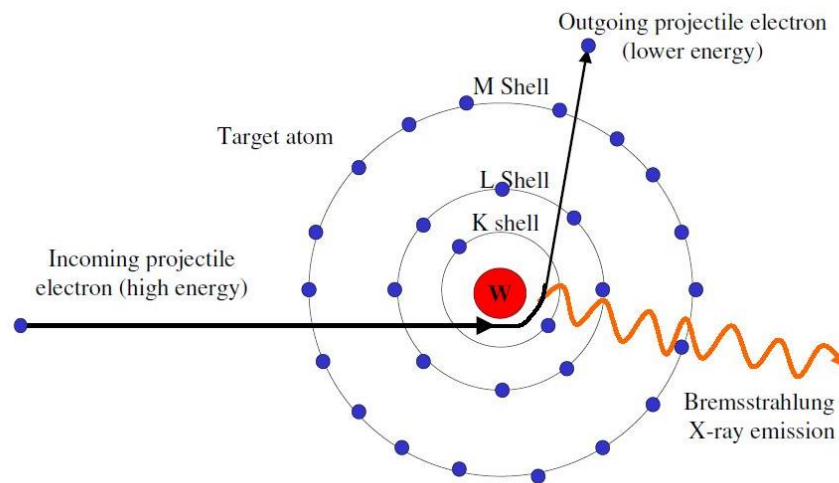
- Filament is Tungsten
- Target typically Tungsten (Alt: Cu, Mo, Ag)
- Window is Beryllium allows X-rays out but keeps chamber under vacuum
- Inefficient process ~1% converted to X-rays

# X-ray Spectrum

## X-ray Spectrum



**Characteristic X-rays**  
(Specific X-rays)



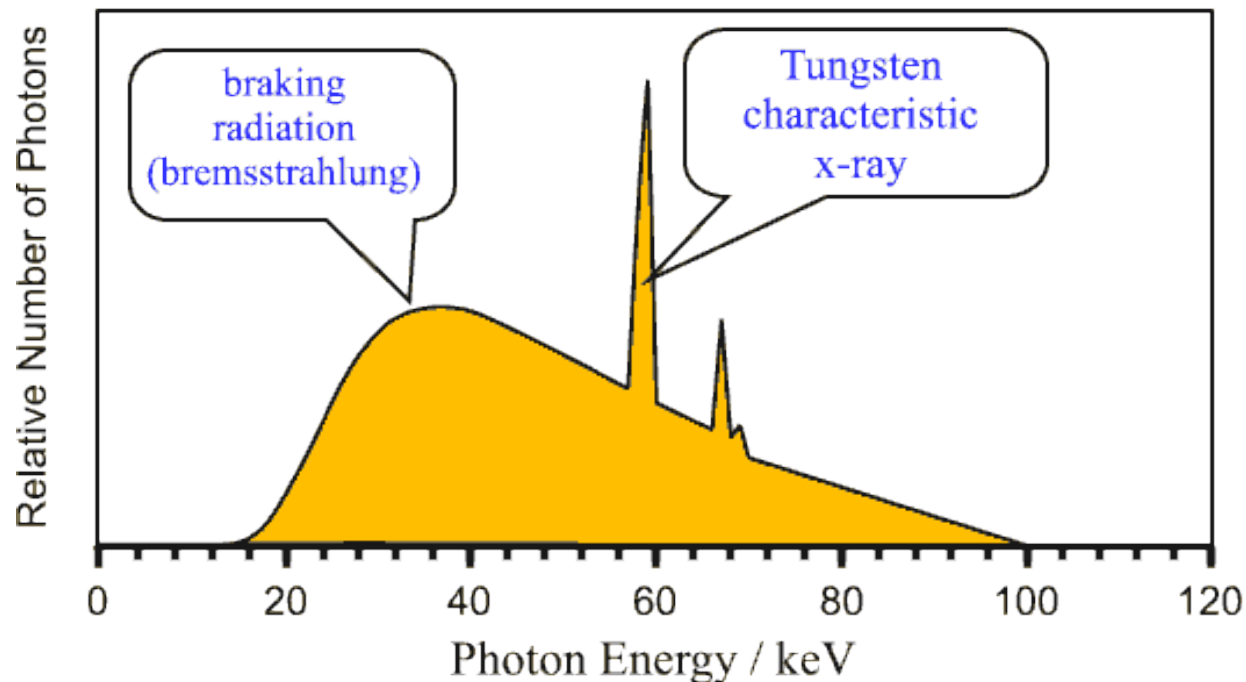
**Bremsstrahlung X-rays**  
(Continuous X-rays)

**X-rays are produced in 2 ways:** Characteristic X-rays (Shell Electron Emission) and Bremsstrahlung X-rays (Incoming Electron Deflection)

# X-ray Spectrum

- **Monochromatic** beam (single energy X-ray). XPS,
- In reality, laboratory X-ray systems are normally a **polychromatic** beam (a range of energy spectrum),
- Various components of the energy spectrum are not attenuated uniformly when passing through an object.
- The lower energy component of X-ray spectrum is more easily attenuated or even completely adsorbed when traveling through a dense part and causes beam hardening defects.

Calculated X-ray Spectrum 100kV, Tungsten target  $13^\circ$  angle



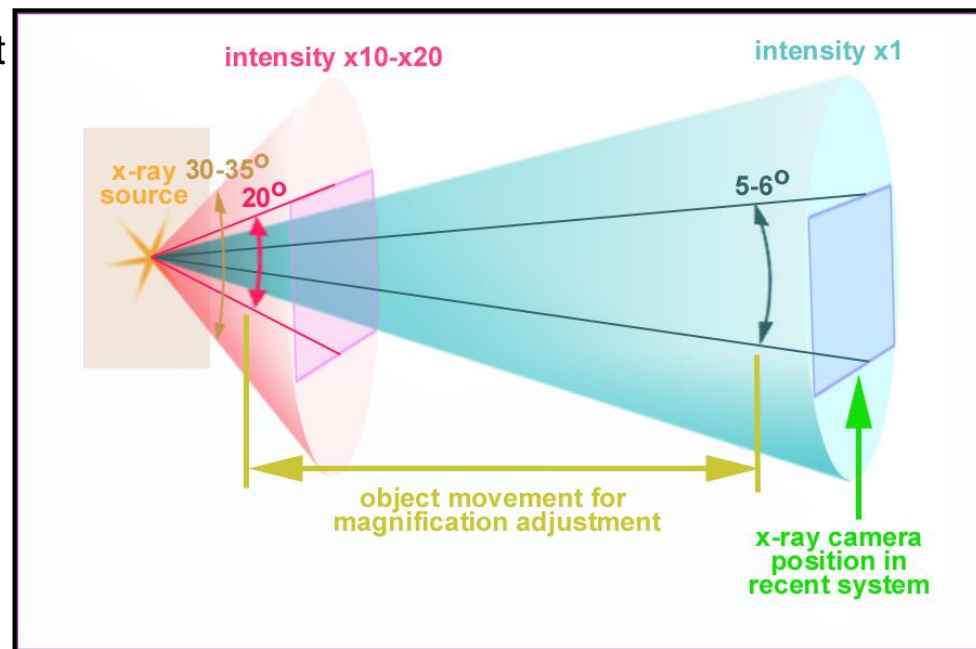
# X-ray Propagation

## X-ray Power



- Total power defined by wattage on target
- $P = I * V$  (Watt = Amps \* Volts)
- $10 \text{ W} = (100\mu\text{A}) * (100\text{kV})$

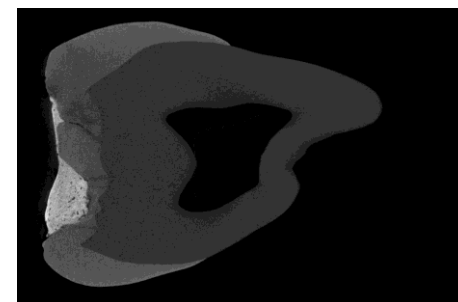
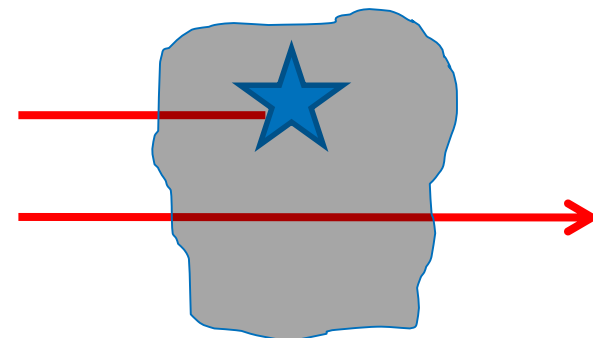
X-ray flux can be thought of like a flow of light.





# X-ray interaction with Matter

- X-rays, like light, are **electromagnetic radiation** but with higher photon energy – and they transmit through materials allowing internal imaging.
- Xray imaging requires **partial absorption** – some x-rays absorbed, some transmitted
- Another requirement for imaging of internal structure by x-rays is **differential absorption**, that is, different parts of the object having significantly different x-ray absorption – to give CONTRAST



# X-ray interaction with Matter

## Attenuation of X-rays

$$I = I_0 * \exp(-\mu x)$$

Where:

$I_0$  = intensity of the unattenuated beam

$x$  = the thickness of (homogenous) material (cm)

$\mu$  = linear attenuation coefficient ( $\text{cm}^{-1}$ )

# Penetration Depth Guidelines

## Typical x-ray penetration depths for the Hamamatsu Microfocus X-ray source assuming a 100 keV accelerated x-ray.

Program reference: P. Bandyopadhyay and C.U. Segre, <http://www.csrii.iit.edu/mucal.html>.  
 Calculations are based on data from: W.H. McMaster N.K. Del Grande, J.H. Mallett and J.H. Hubbell, "Compilation of x-ray cross sections", Lawrence Livermore National Laboratory Report UCRL-50174 (section I 1970, section II 1969, section III 1969 and section IV 1969).

1	1																	18	
1	H																	2	He
2	3	4											5	6	7	8	9	10	
2	Li	Be											B	C	N	O	F	Ne	
	14 cm	4 cm											3.08 cm	2.938 cm	N				
3	11	12											13	14	15	16	17	18	
3	Na	Mg											Al	Si	P	S	Cl	Ar	
	6.4 cm	3.37 cm											2.18 cm	2.34 cm	2.97cm	2.49 cm			
4	19	20	21	22	23	24	25	26	27	28	29	30	31	32	33	34	35	36	
4	K	Ca	Sc	Ti	V	Cr	Mn	Fe	Co	Ni	Cu	Zn	Ga	Ge	As	Se	Br	Kr	
	5.06 cm	2.51 cm	1.33 cm	0.812 cm	0.574 cm	0.44 cm	0.40 cm	0.367 cm	0.292 cm	0.264 cm	0.246 cm	0.286 cm	0.334 cm	0.35 cm	0.301 cm	0.330 cm	0.467 cm		
5	37	38	39	40	41	42	43	44	45	46	47	48	49	50	51	52	53	54	
5	Rb	Sr	Y	Zr	Nb	Mo	Tc	Ru	Rh	Pd	Ag	Cd	In	Sn	Sb	Te	I	Xe	
	0.85 cm	0.475 cm	0.245 cm	0.162 cm	0.112 cm	876 μm	761 μm	663 μm	620 μm	615 μm	651 μm	760 μm	843 μm	0.113 cm	828 μm	903 μm	0.103 cm		
6	55	56	57-71	72	73	74	75	76	77	78	79	80	81	82	83	84	85	86	
6	Cs	Ba	La-Lu	Hf	Ta	W	Re	Os	Ir	Pt	Au	Hg	Tl	Pb	Bi	Po	At	Rn	
	0.255 cm	0.129 cm	Lanthanide	180 μm	142 μm	116 μm	101 μm	94 μm	93 μm	95 μm	101 μm	143 μm	155 μm	161 μm	175 μm			16.8 cm	
7	87	88	89-103	104	105	106	107	108	109										
7	Fr	Ra	Ac-Lr	Rf	Db	Sg	Bh	Hs	Mt										
			Actinide																
<b>LANTHANIDE</b>																			
6	57	58	59	60	61	62	63	64	65	66	67	68	69	70	71				
	La	Ce	Pr	Nd	Pm	Sm	Eu	Gd	Tb	Dy	Ho	Er	Tm	Yb	Lu				
	702 μm	606 μm	574 μm	539 μm	531 μm	463 μm	629 μm	397 μm	376 μm	352 μm	318 μm	306 μm	285 μm	359 μm	253 μm				
<b>ACTINIDE</b>																			
7	89	90	91	92	93	94	95	96	97	98	99	100	101	102	103				
	Ac	Th	Pa	U	Np	Pu	Am	Cm	Bk	Cf	Es	Fm	Md	No	Lr				
		477 μm		276 μm		254 μm													

To be used only as a rough guide. These values do not represent limits only an estimate of the thickness of material needed to obtain ~33% transmission

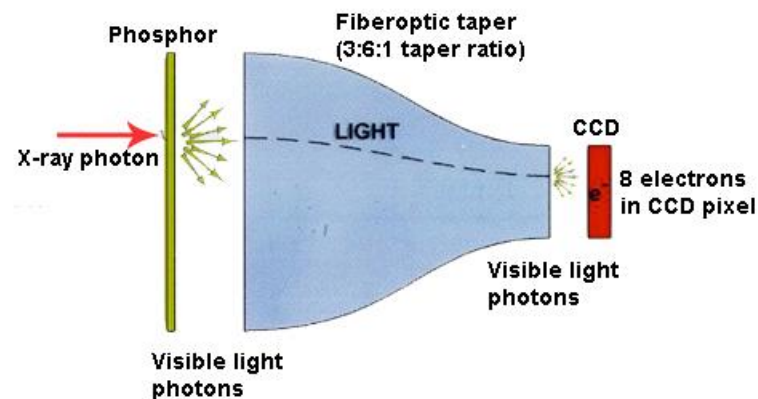
Table courtesy of B. Patterson, Los Alamos National Laboratory.

# X-ray Image Detection

## Scintillators and Detectors

**Scintillators** convert X-ray photons into white light that can be imaged by the detector (CCD or CMOS),

**Detectors** convert white light into electrical charge which is read out through the camera as pixel value.



Metal Oxide Semiconductor (MOS) Capacitor

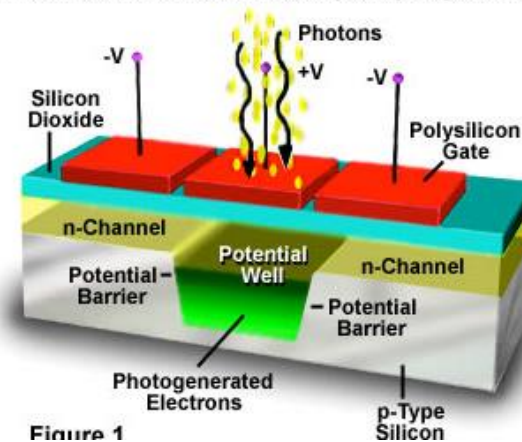


Figure 1



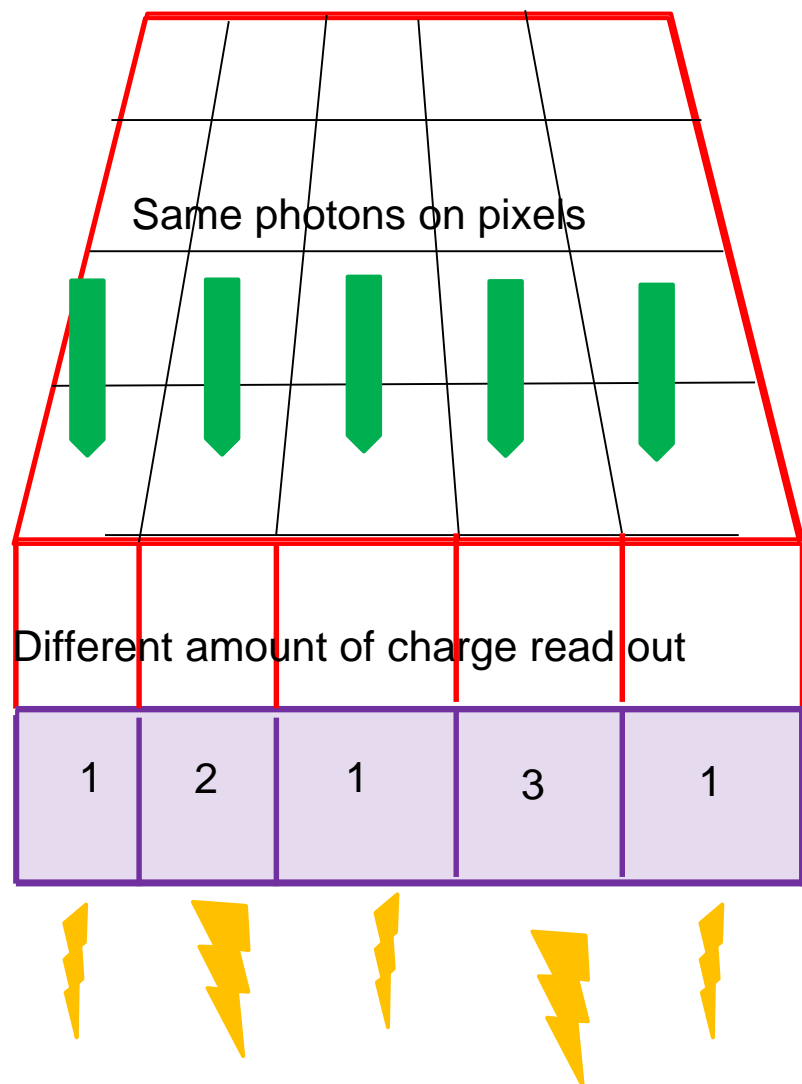
# X-ray Image Detection

## Pixel Readout Noise

Each pixel has readout noise.

Readout noise occurs from fluctuation in the amplification of digitizing the analog signal.

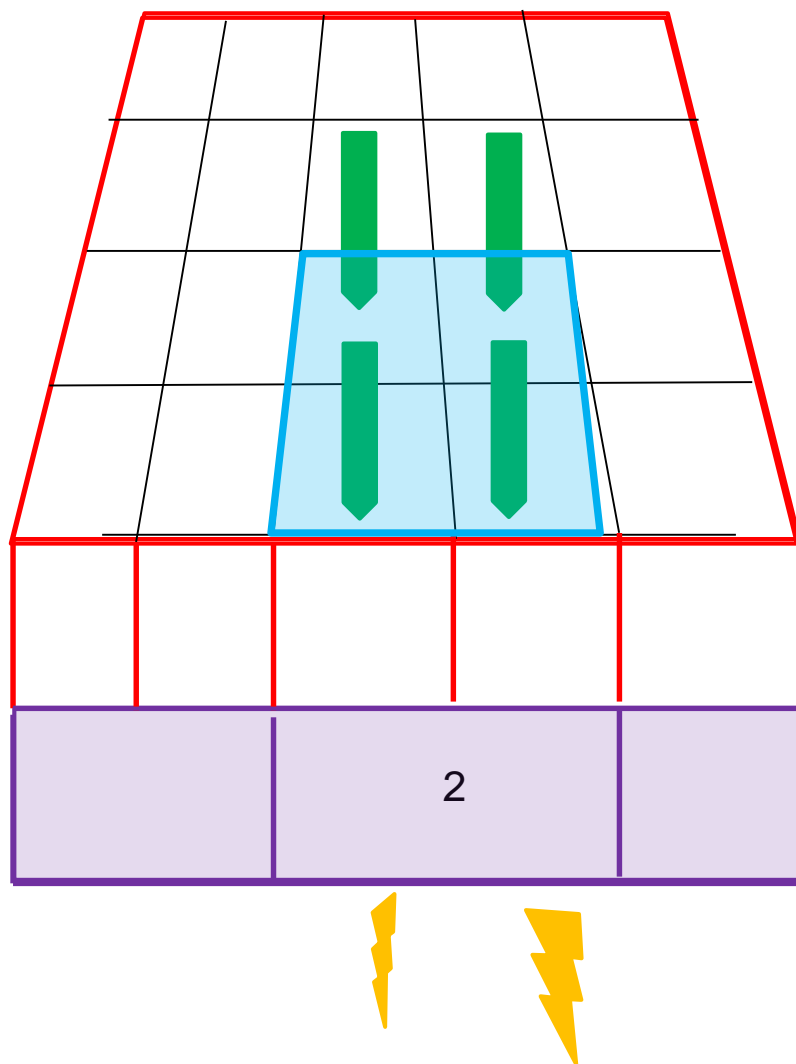
(i.e. even though same amount of charge is put on each pixel, the Analog-to-Digital Units (ADU) is not the same.



# X-ray Image Detection

## Reduce Readout Noise

By binning the pixel, it reduces readout noise, in case of 2 x 2 binning, because it is signal from 4 pixel with 1 readout, so the contribution is much less.

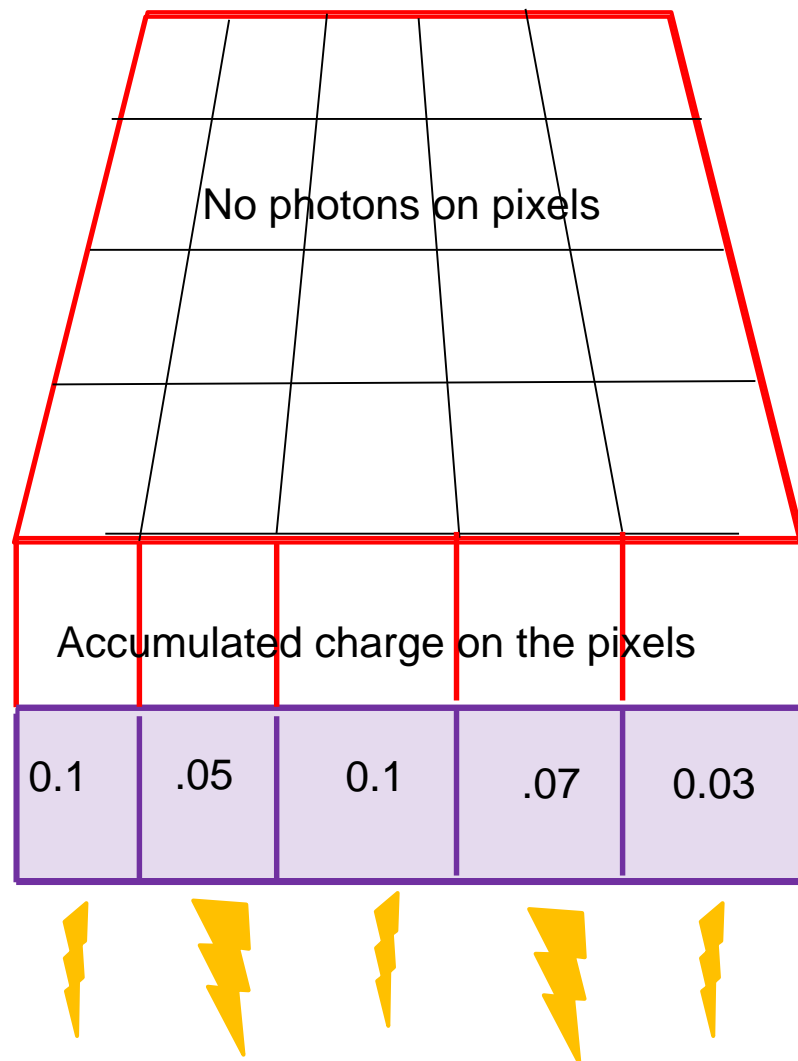


# X-ray Image Detection

## Dark Current

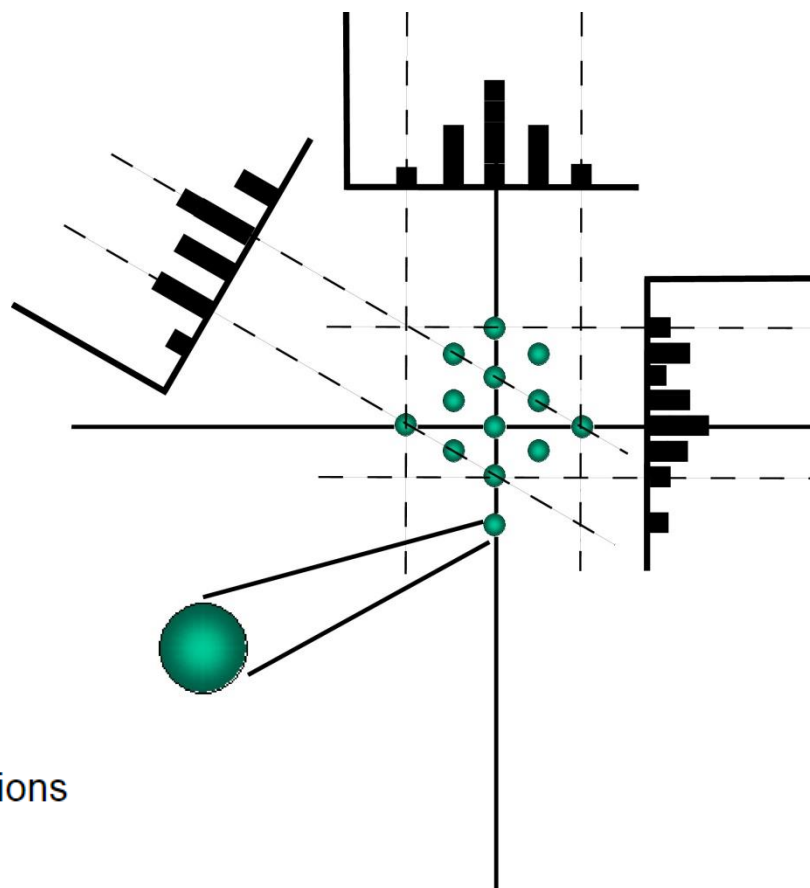
Dark current is accumulated charge on the detector in the absence of light.

## FLAT FIELDS



# Computed Tomography Reconstruction

## Ideal Case of Uniform Attenuating Sphere



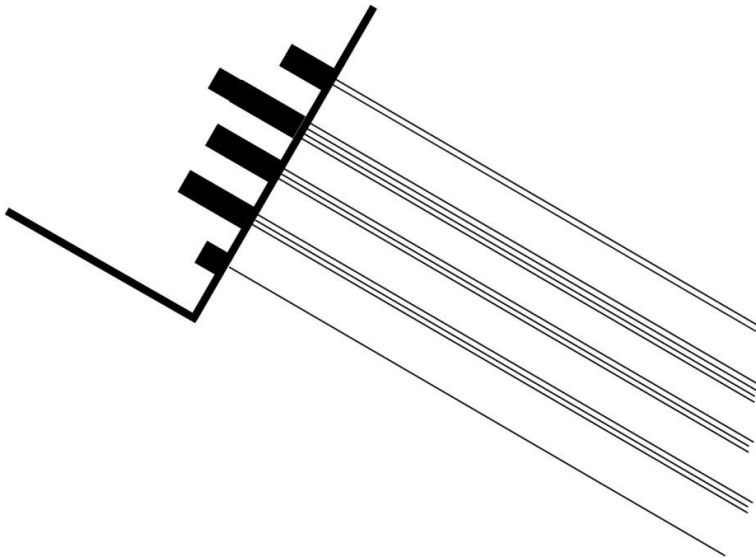
### Assumptions:

- Ideal Geometry
- Low Noise
- Sufficient number of projections

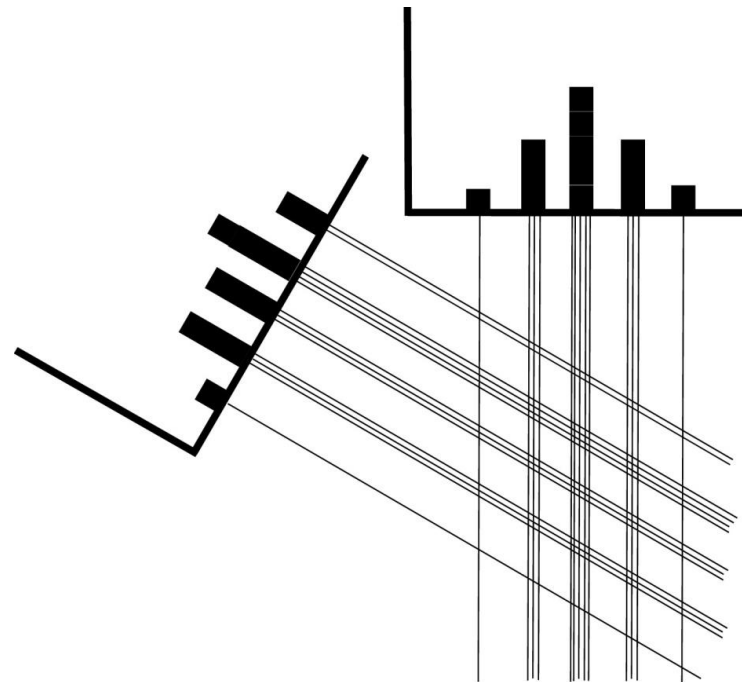


# Computed Tomography Reconstruction

Ideal Case of Uniform Attenuating Sphere



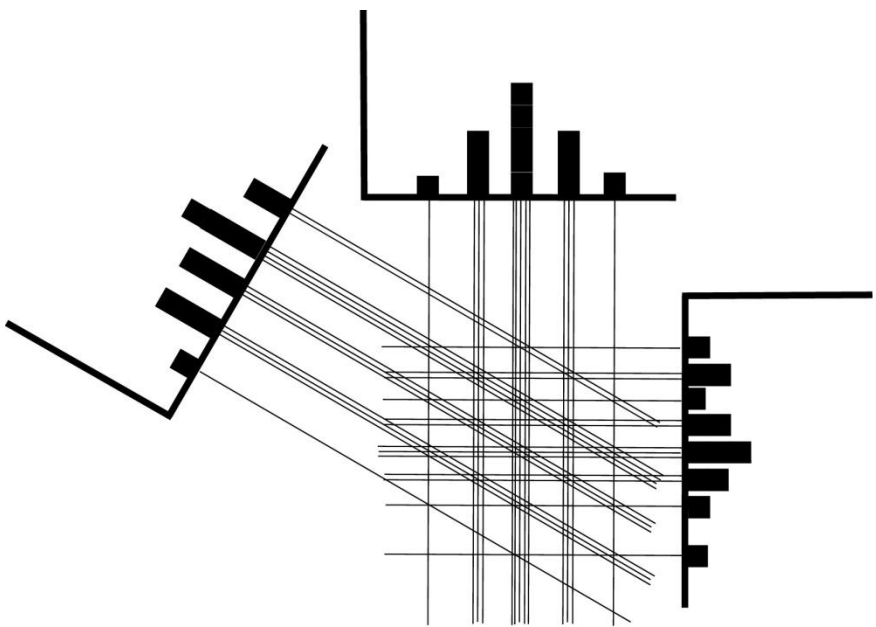
First Projection



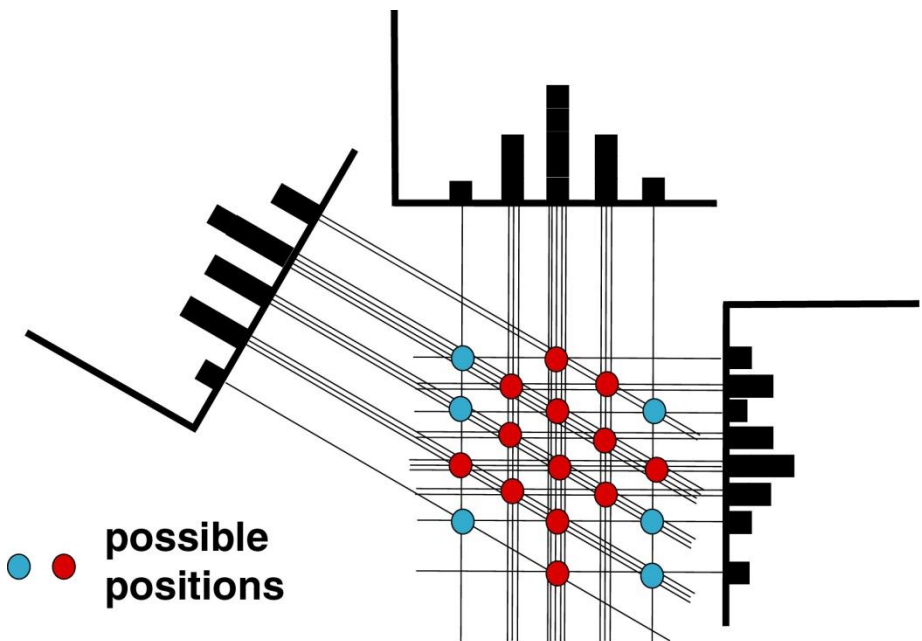
Second Projection

# Computed Tomography Reconstruction

## Ideal Case of Uniform Attenuating Sphere



First Projection

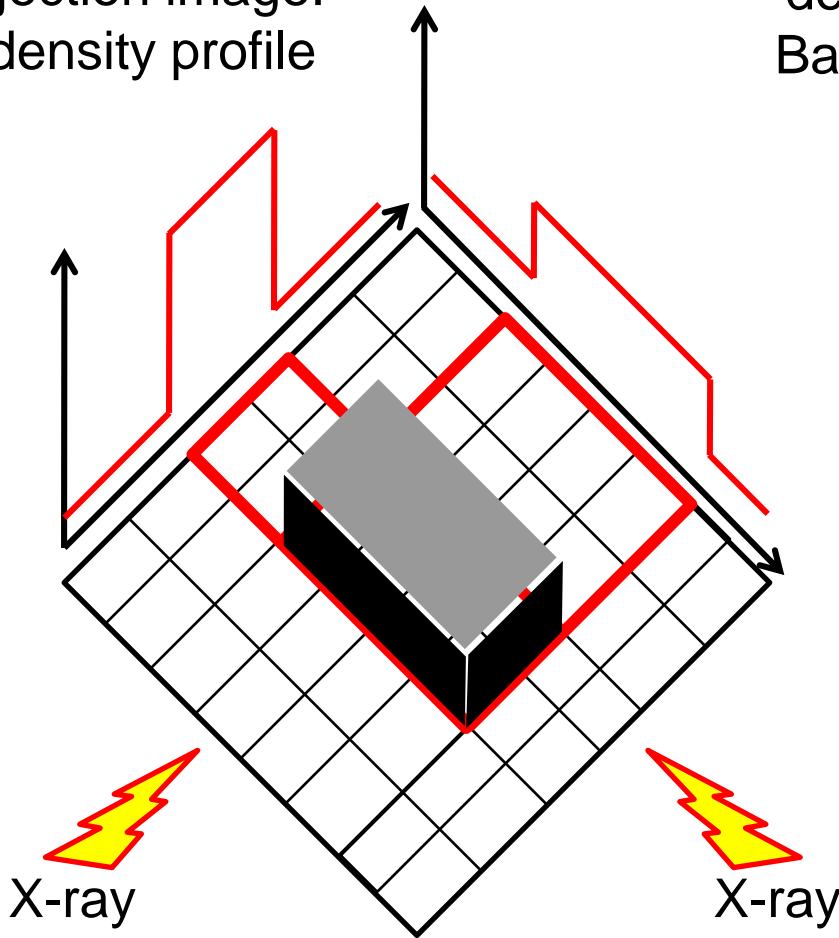


Second Projection

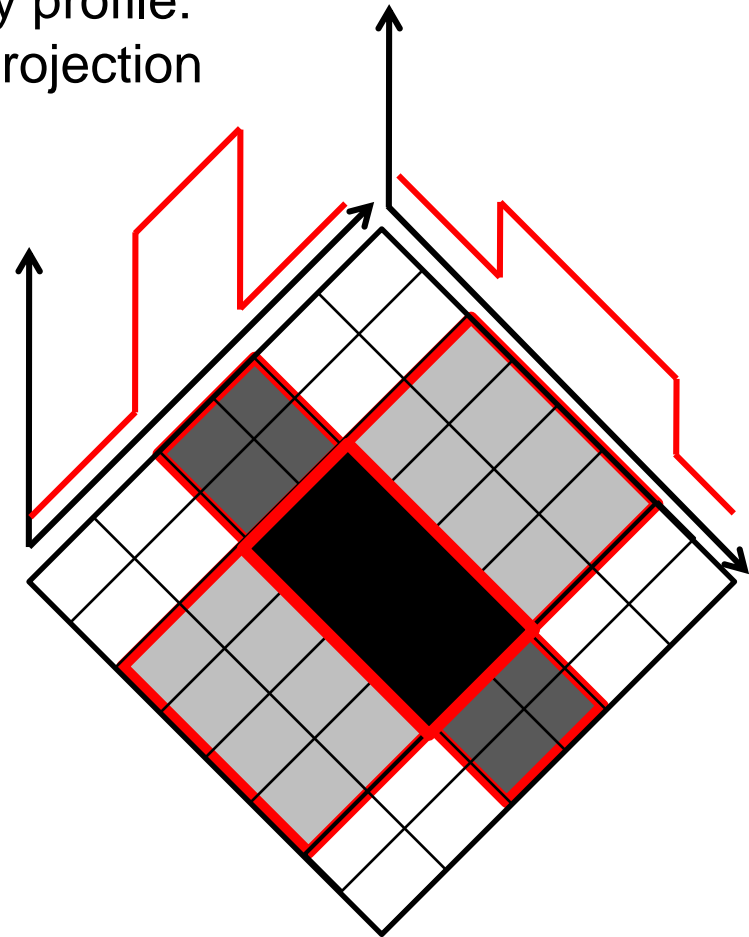
● ● possible positions

# Reconstruction: back projection

Projection image:  
density profile



density profile:  
Back projection

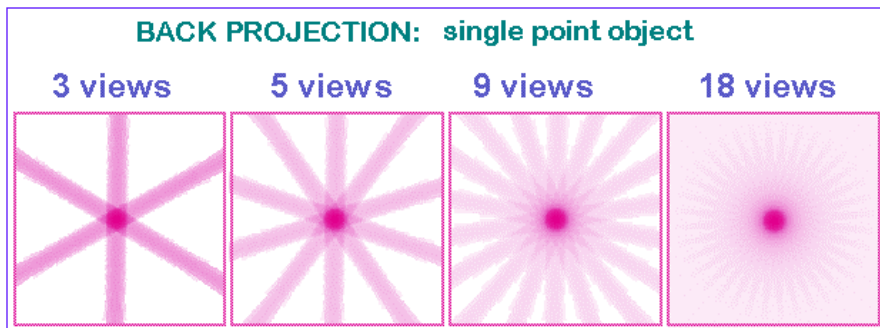


# Computed Tomography Reconstruction

## Backprojection

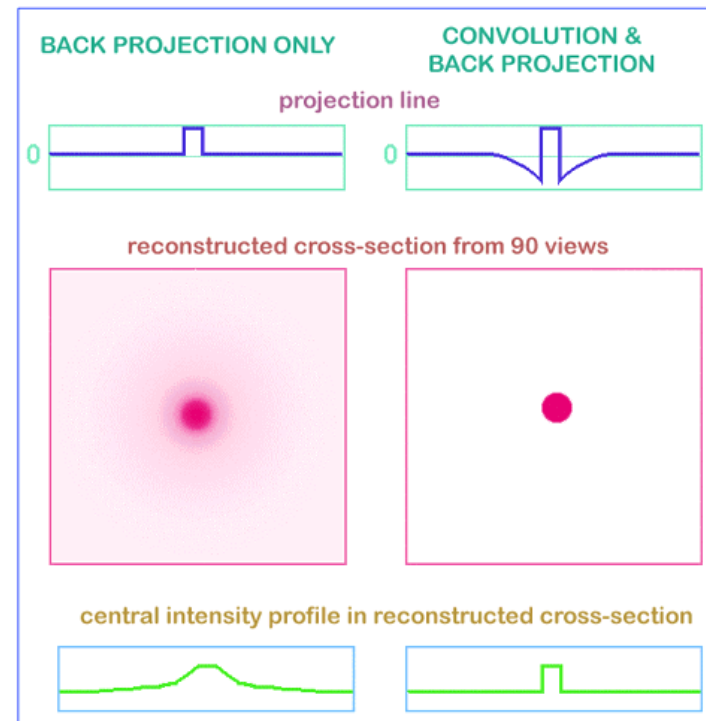
Modified Feldkemp Backprojection (NRECON SERVER)

INSTARECON: Proprietary that makes use of oversampling in the center to speed reconstruction up



## Convolution

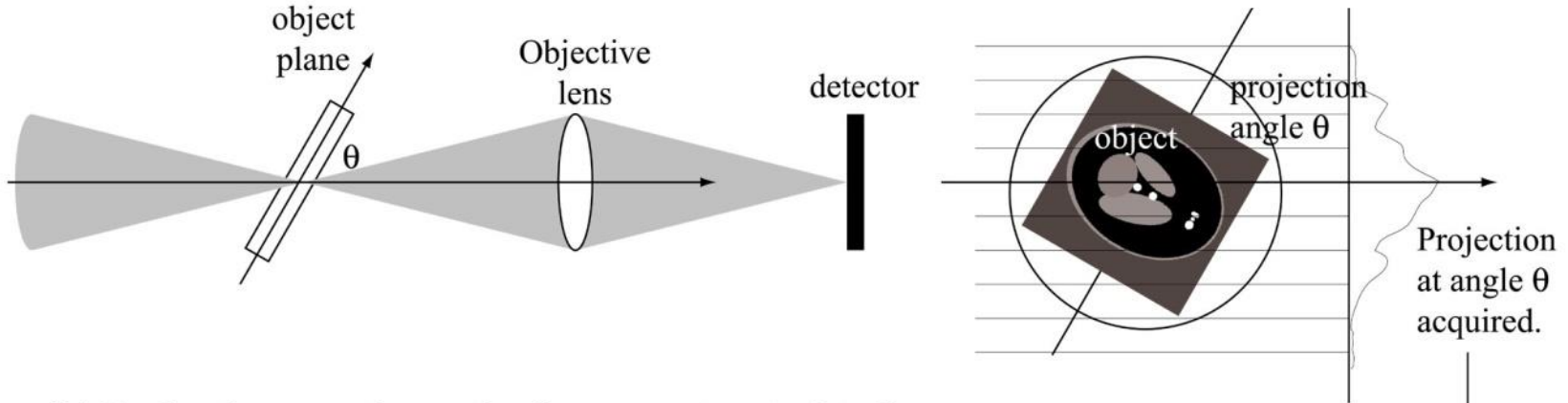
Applies a sharpening correction to the results of back-projection



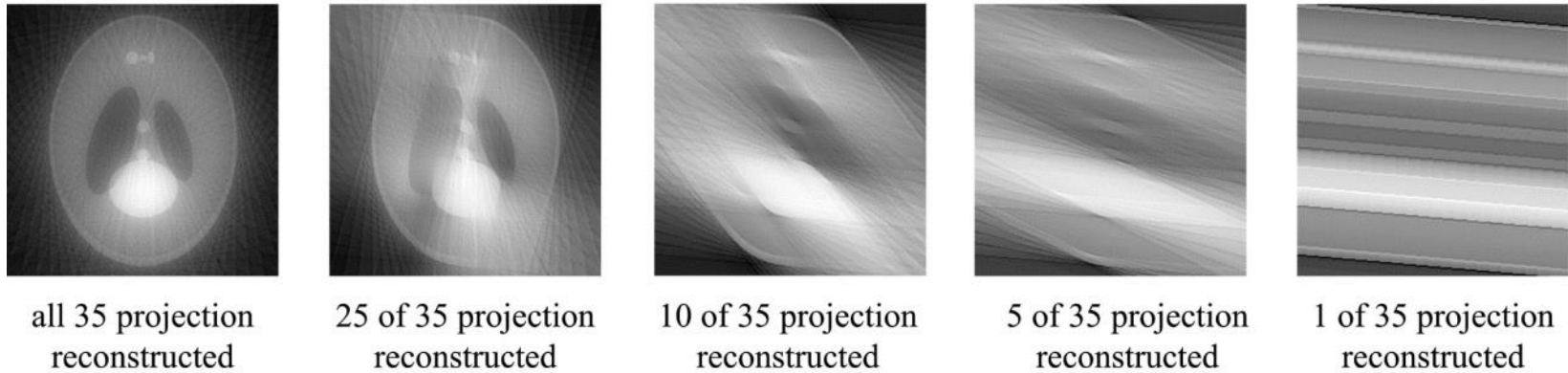


# Computed Tomography Reconstruction

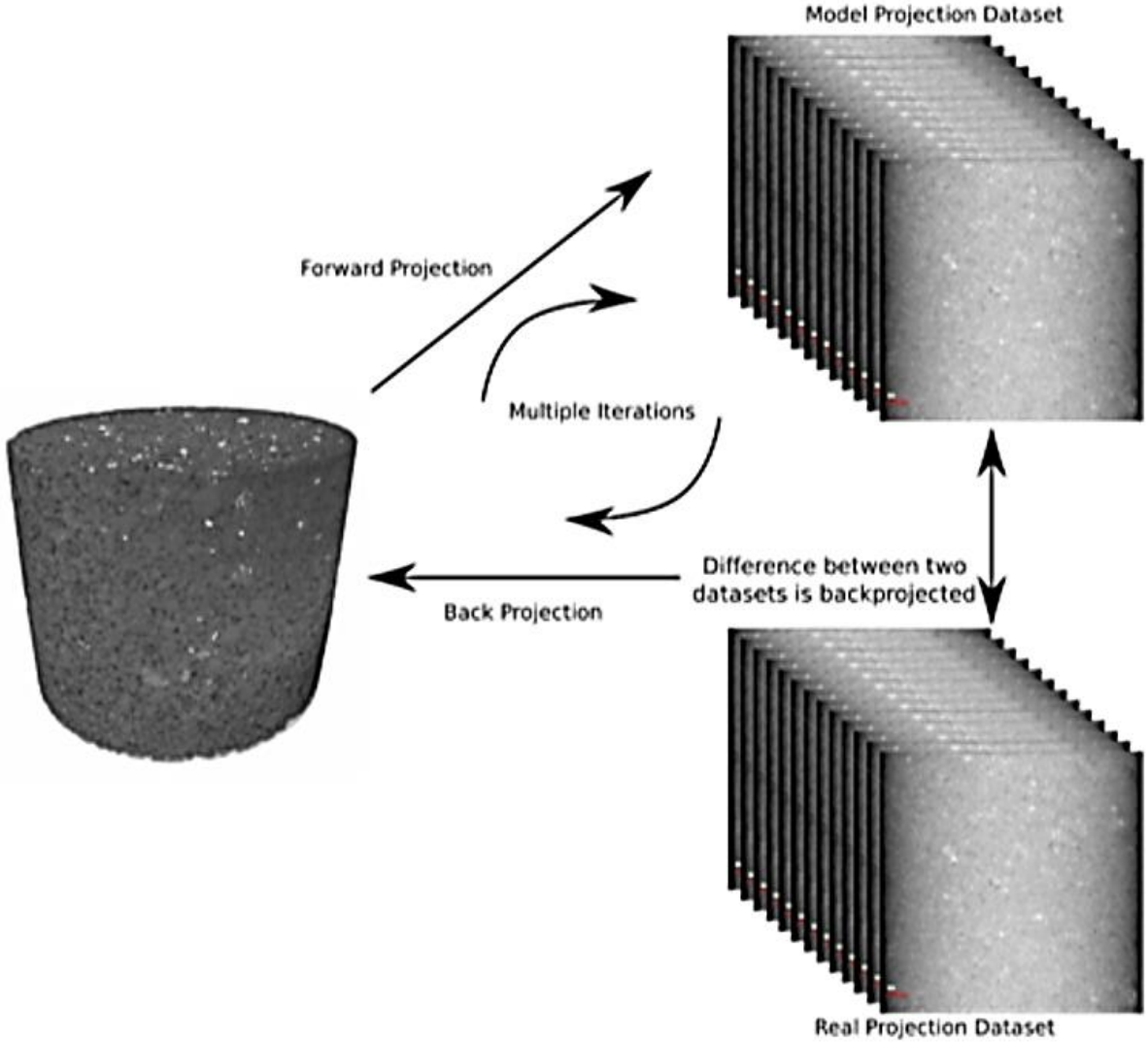
(a) Object imaged at various angles to obtain tomographic projections



(b) Projections mathematically reconstructed to form a 3D volume image that represents the original object.

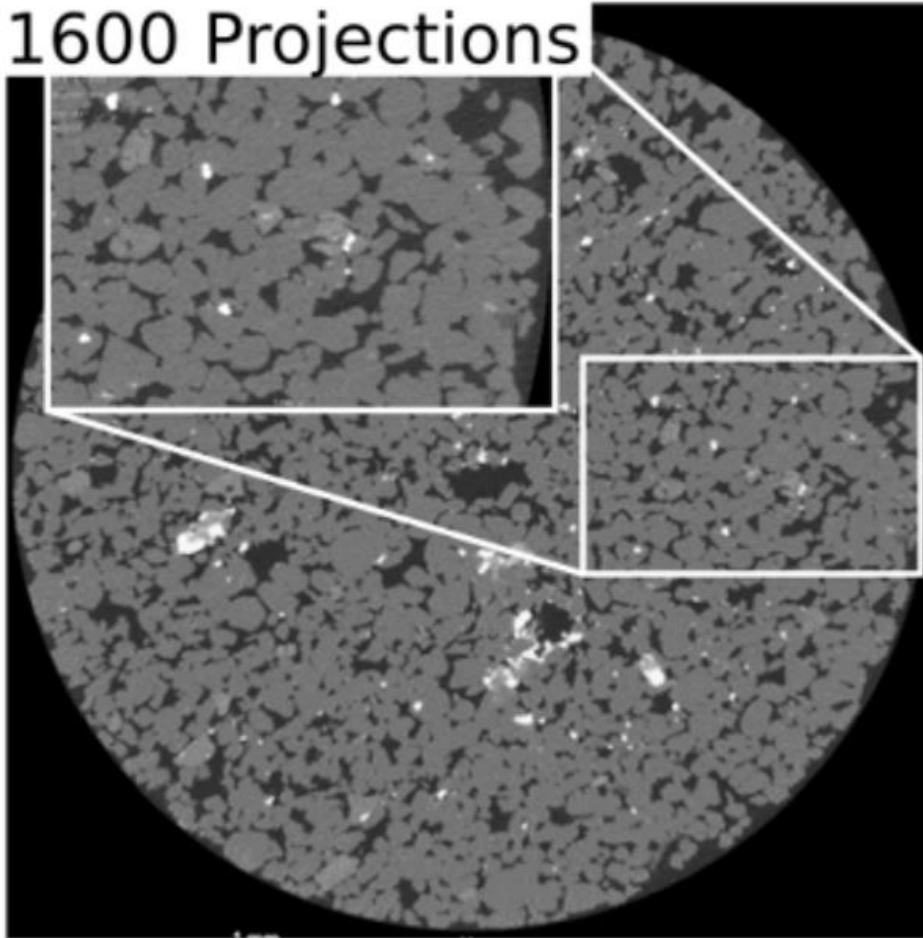


# Iterative Reconstruction



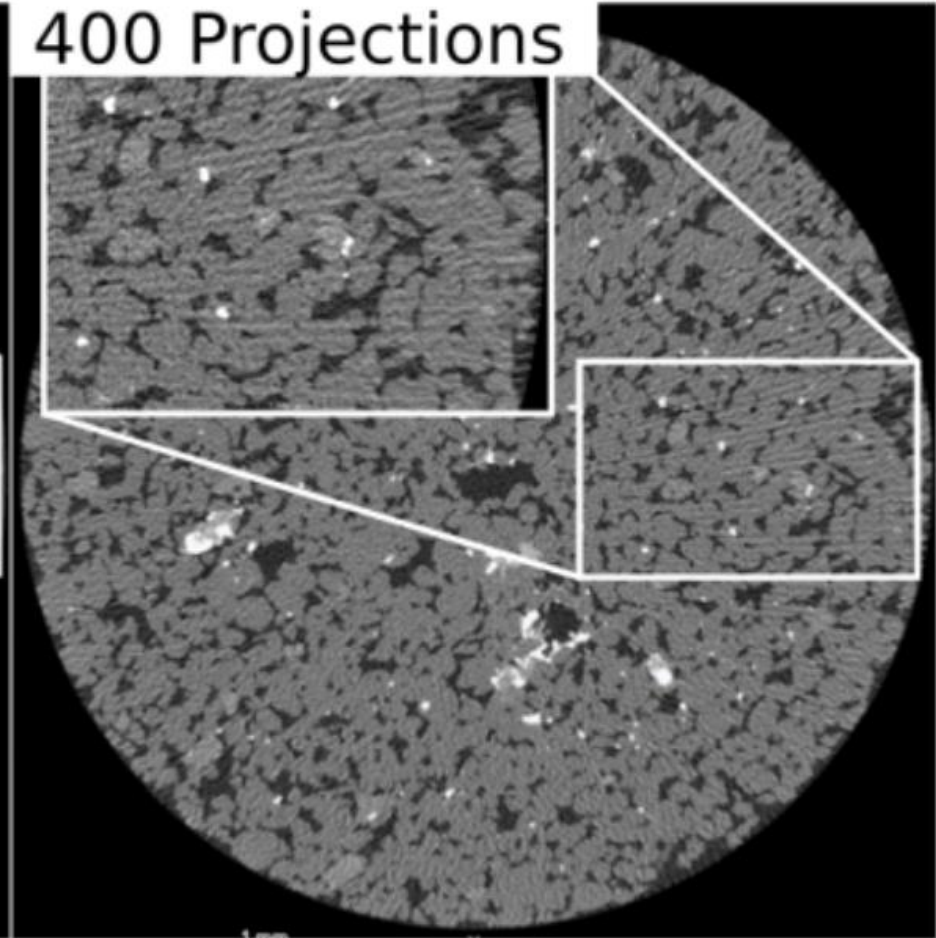
# Back Projection

1600 Projections



9mm

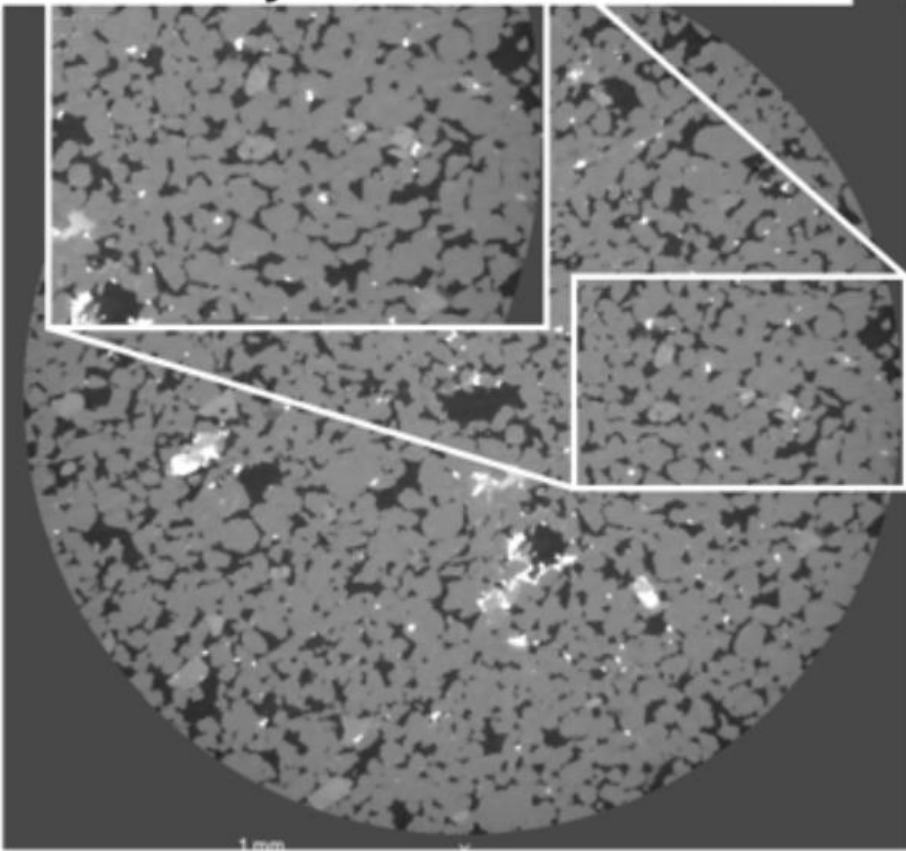
400 Projections



9mm

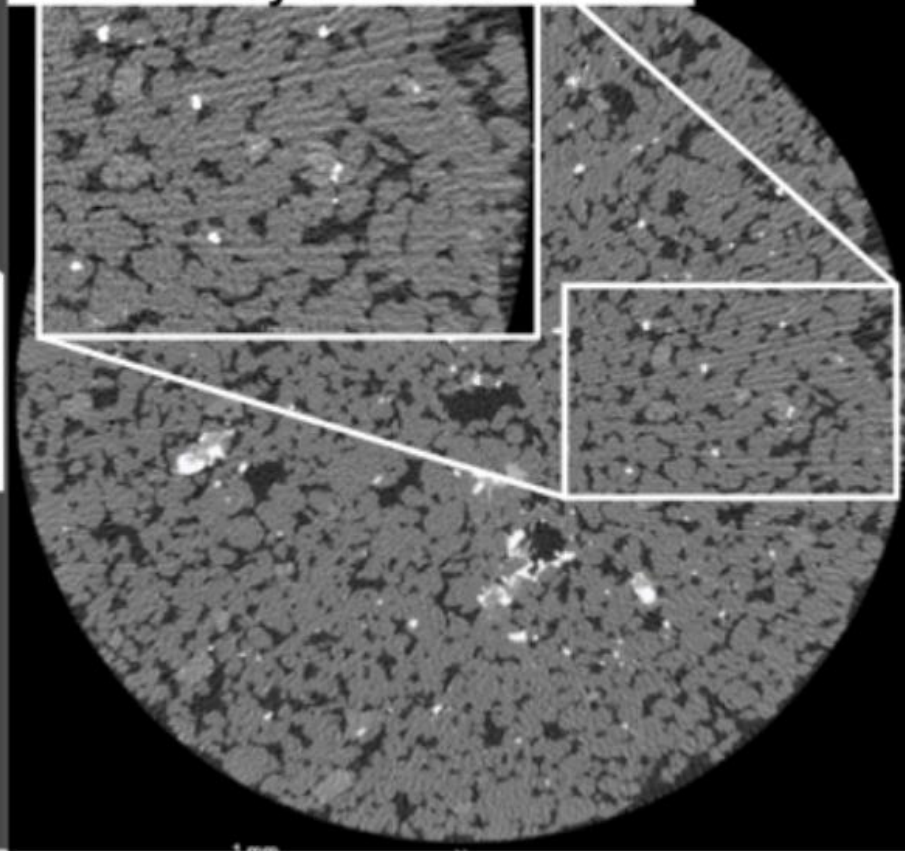
# BP vs. Iterative Reconstruction

400 Projections Iterative



9mm

400 Projections FBP

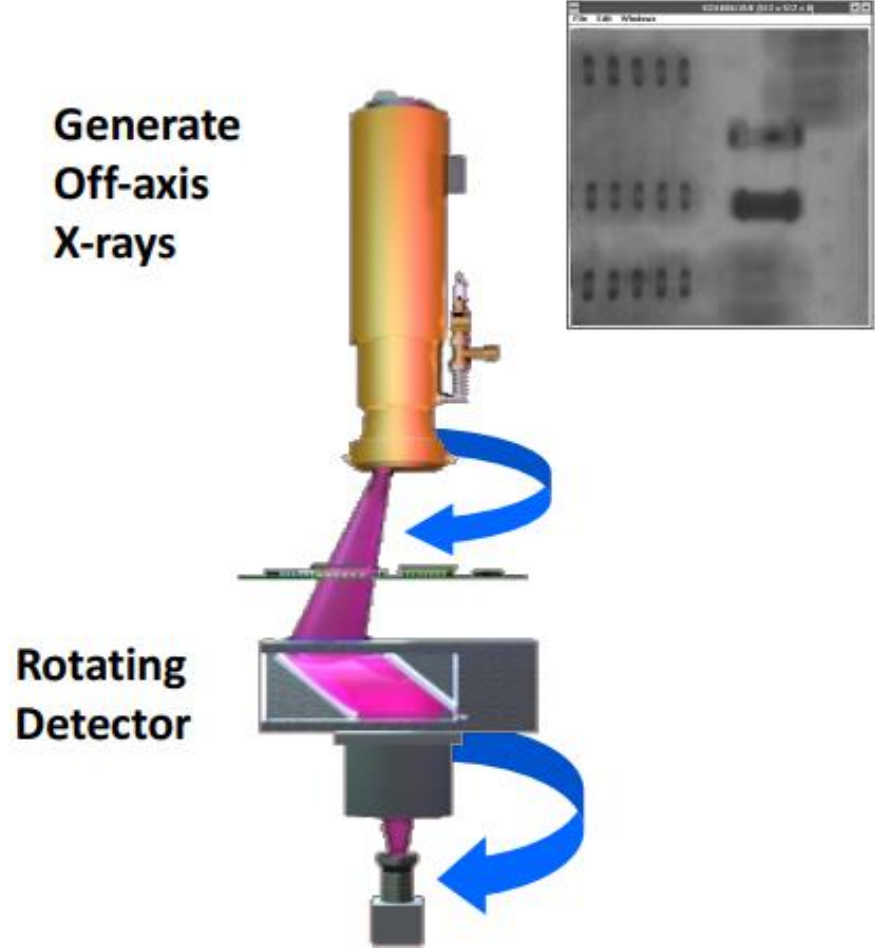


9mm

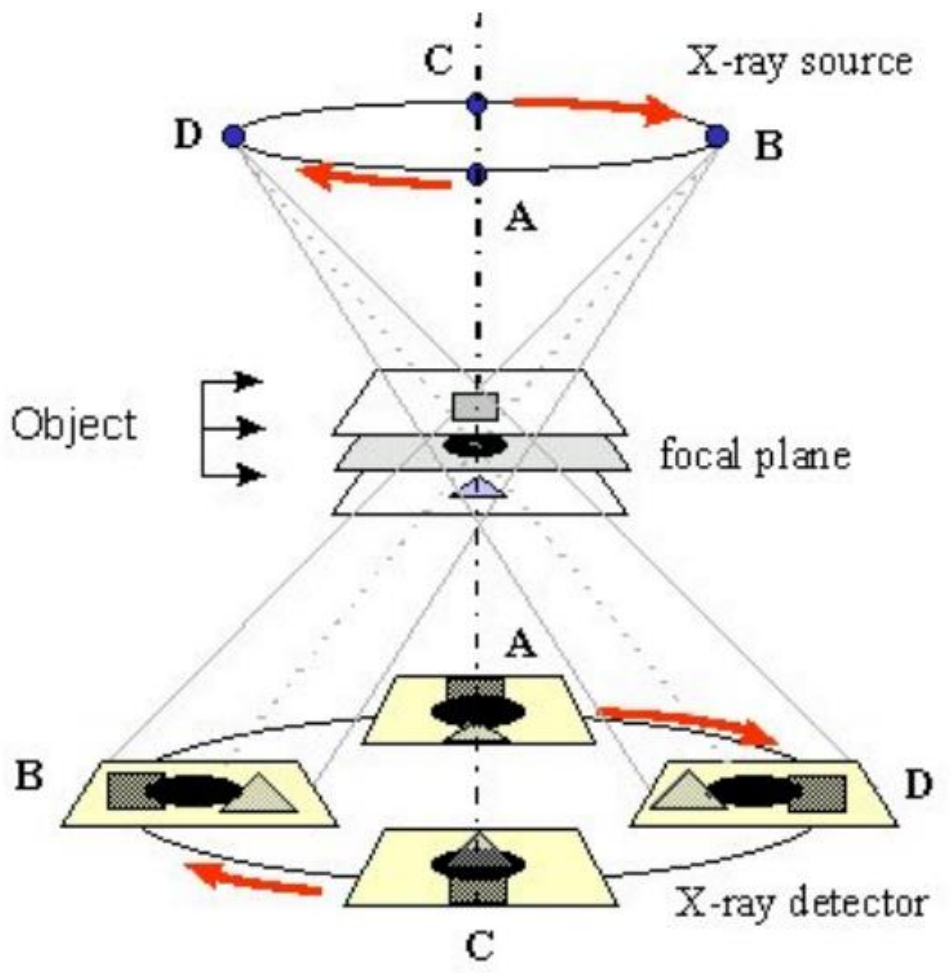


# X-ray Laminography

Mechanical Image Integration



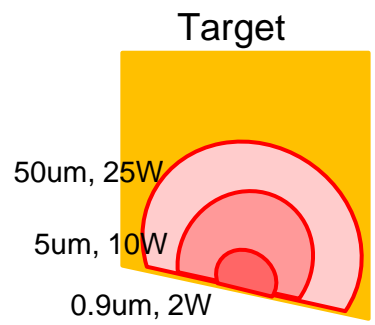
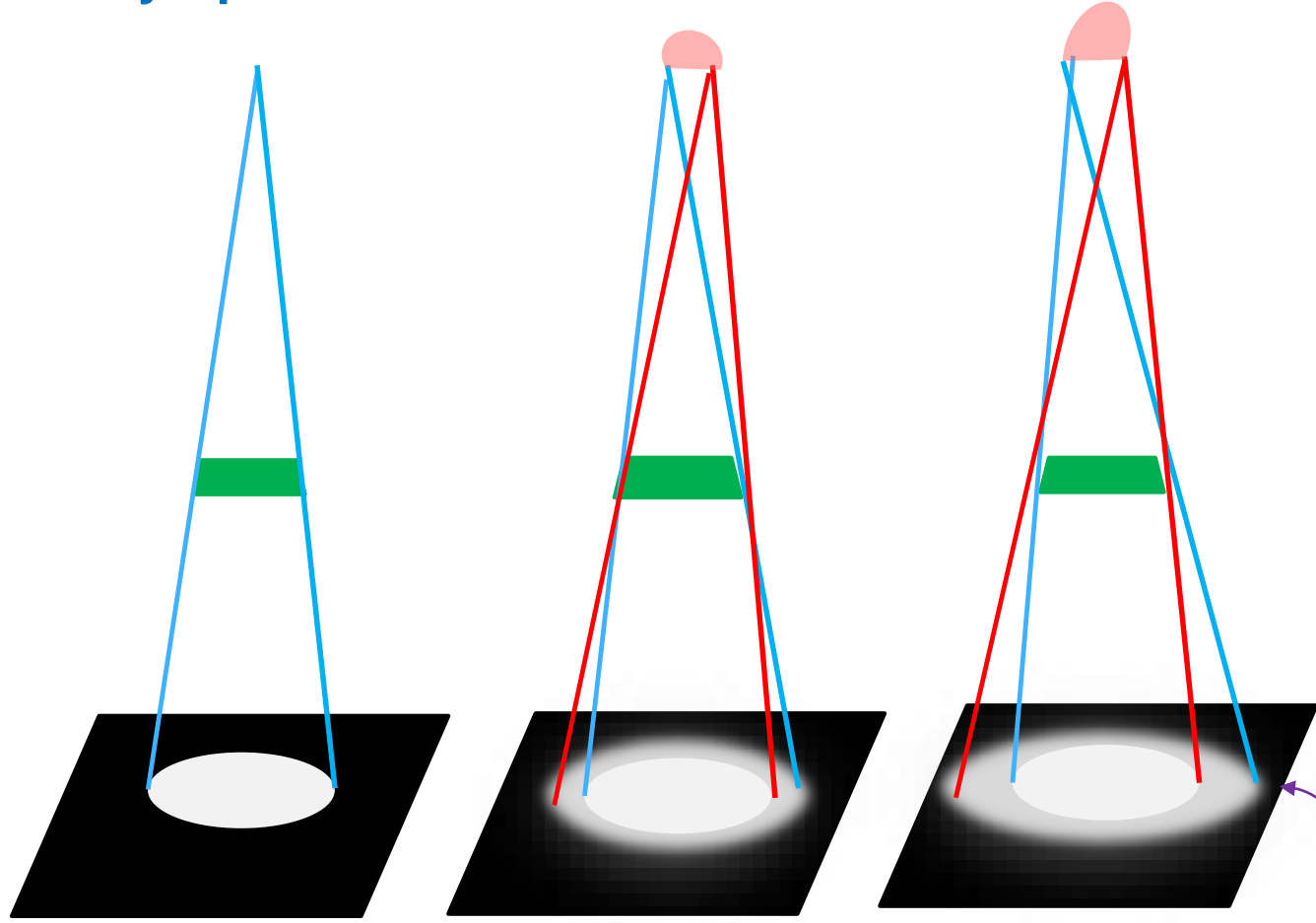
Principle of Laminography



# Geometrical Magnification



## X-ray Spot Size



The smaller the spot size, the harder it is to get more X-ray power out.

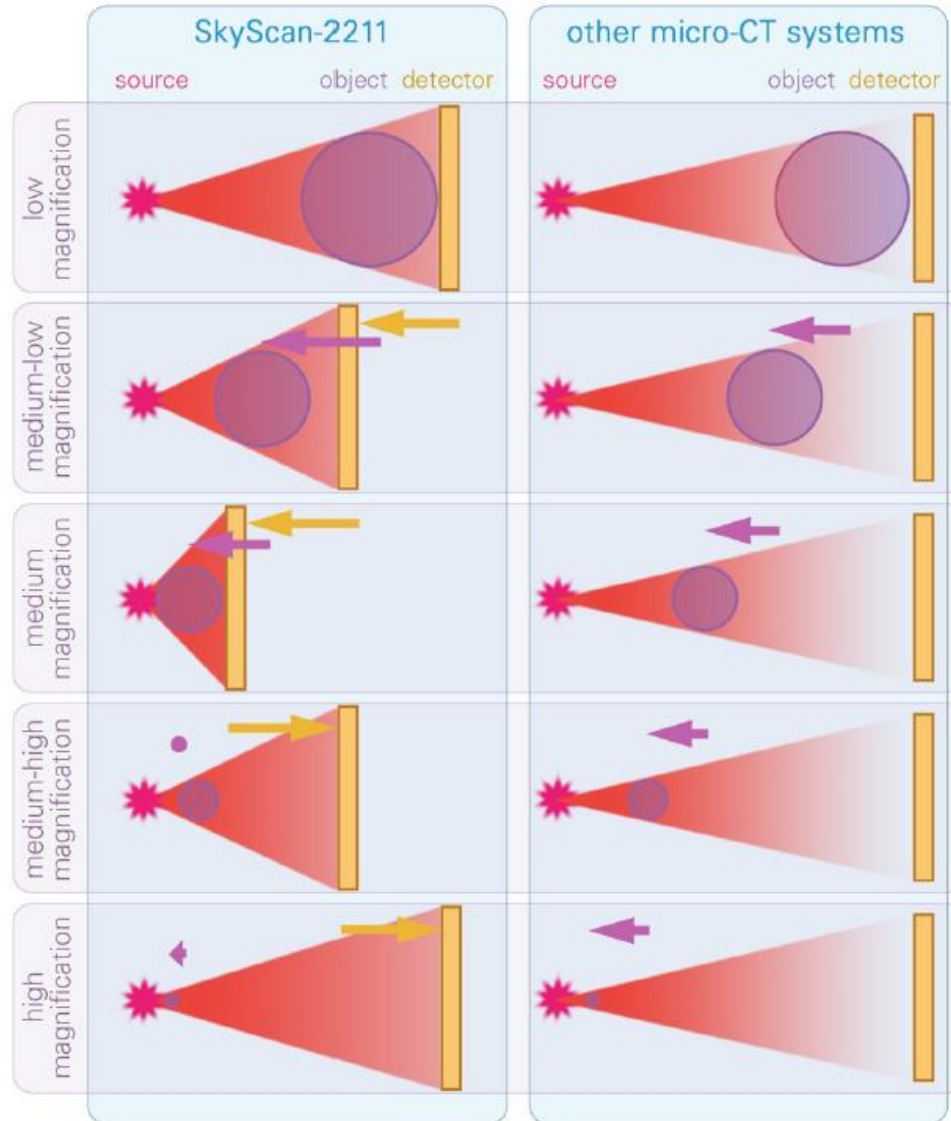
Or vice versa, the more power applied to the source, the larger the spot size is.

Penumbra Blurring

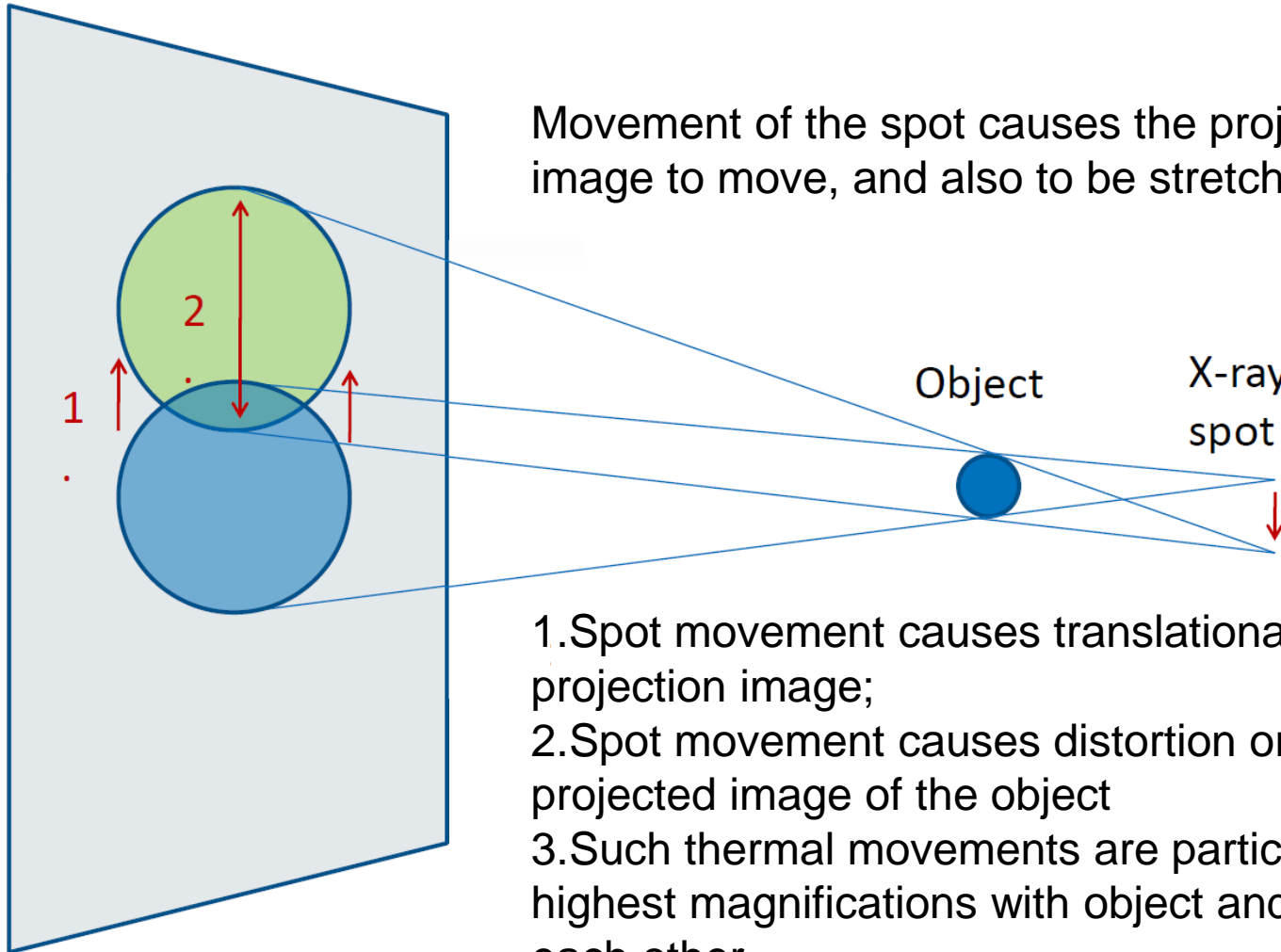




# Geometrical Magnification

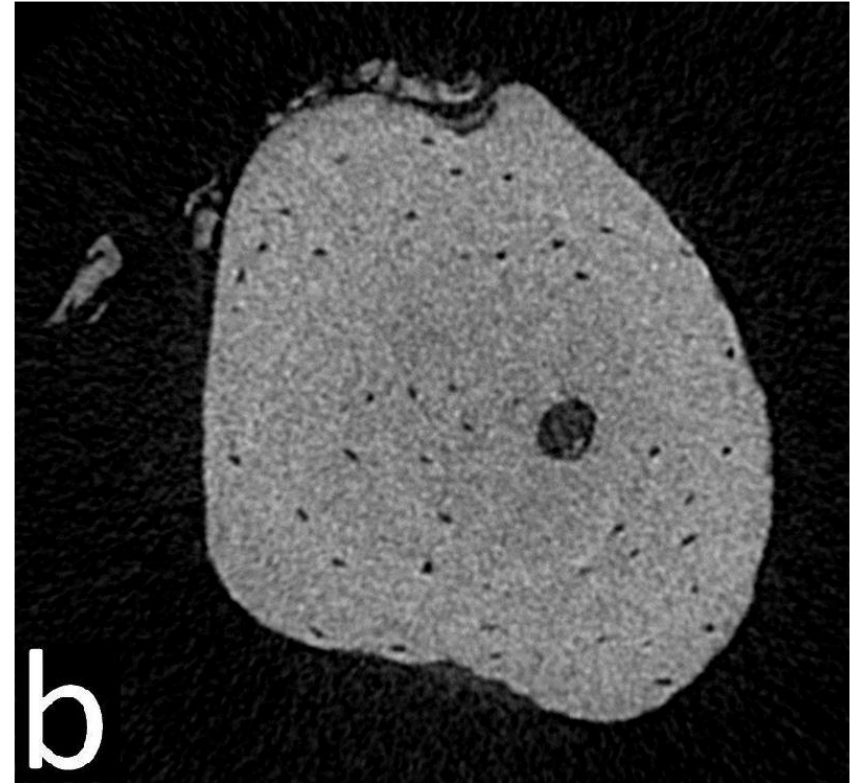
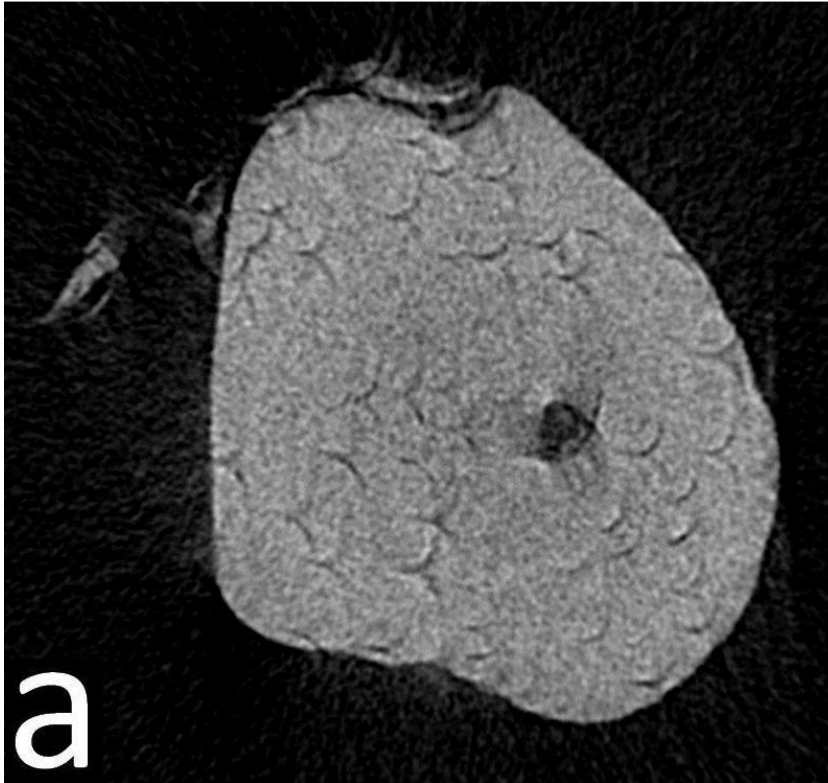


# Alignment Correction

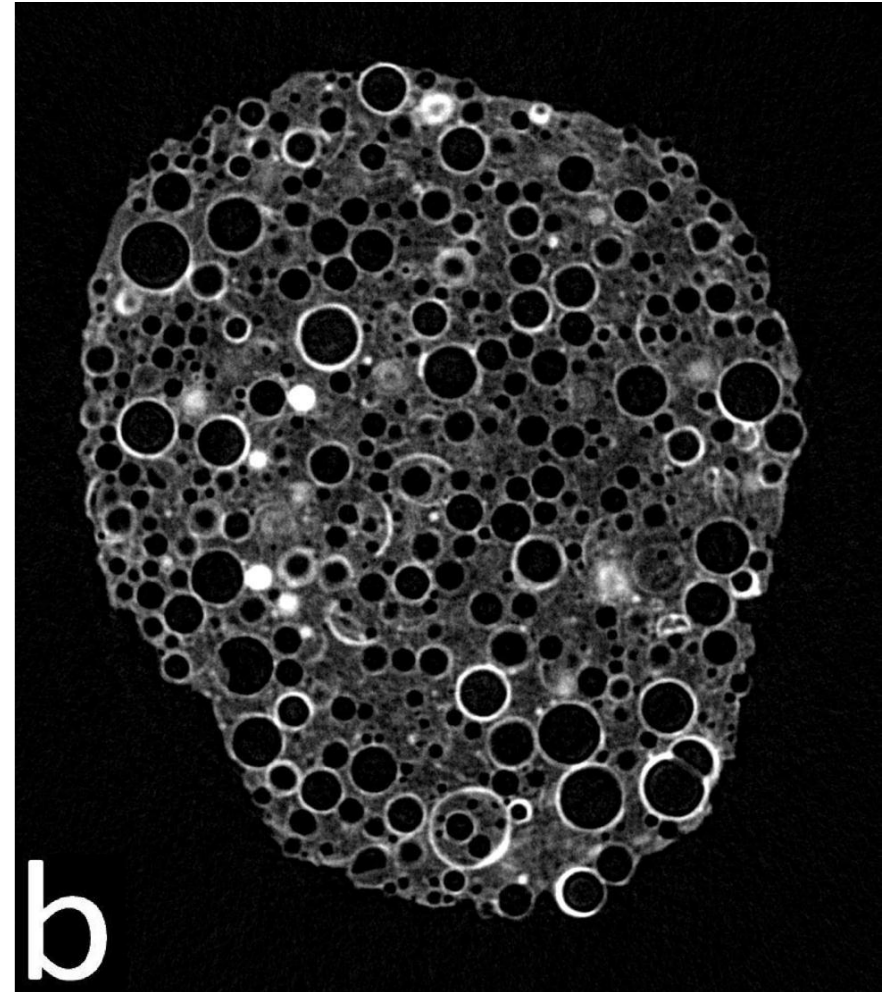
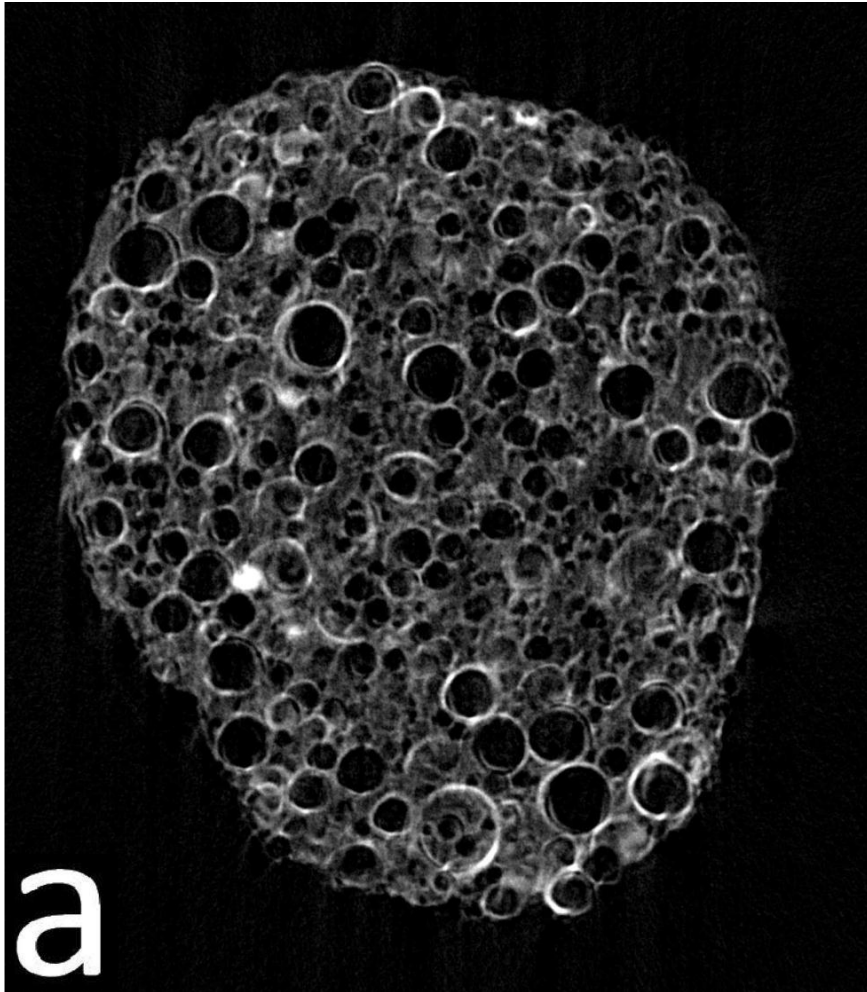


1. Spot movement causes translational movement of the projection image;
2. Spot movement causes distortion or stretching of the projected image of the object
3. Such thermal movements are particularly severe at the highest magnifications with object and source very close to each other.

# Alignment Correction



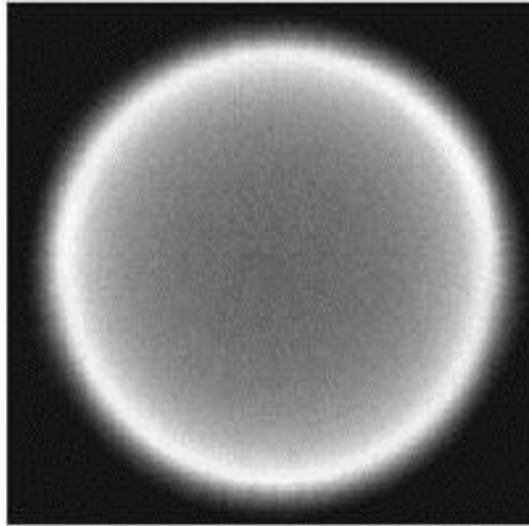
# Alignment Correction



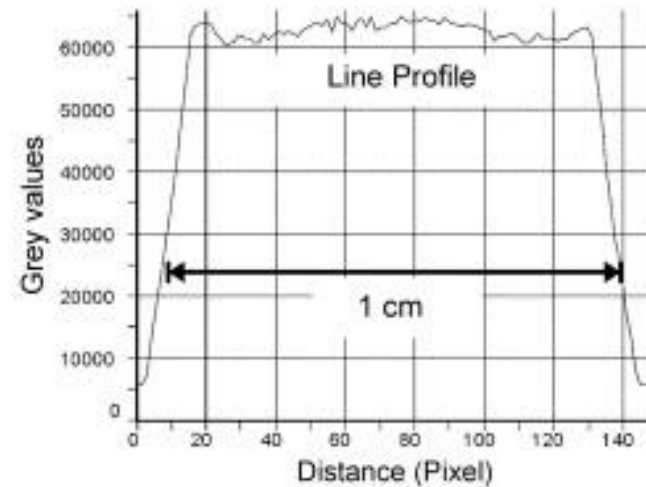
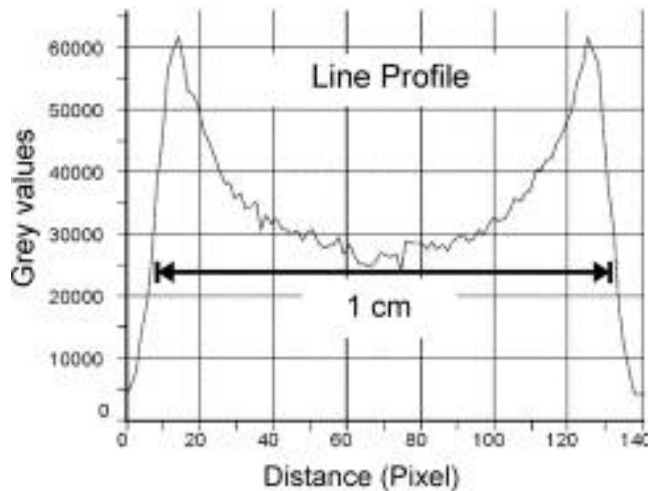
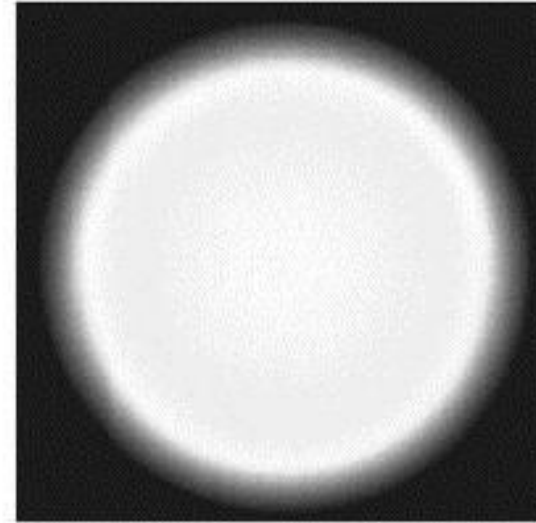


# Beam Hardening Correction

Before



After



# X-ray Scanners



Zeiss



Skyscan



Nikon



Nikon



Nordson



Creative Electron